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# FORMULATION AND EVALUATION OF BUCCO-ADHESIVE TABLET OF ANTI-DIABETIC AGENT.

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**Abstract:** - The goal of this work was to investigate and describe mucoadhesive buccal tablets of pioglitazone hydrochloride utilising a variety of bioadhesive polymers in combination, including sodium alginate, carbopol, HPMC K4M, and HPMC K15M. TEN formulations were created with various polymer concentrations and combinations of two polymers in each formulation. Individual polymers make up formulations F1 to F4. F5 to F10 were made up of two polymer combinations. Physicochemical criteria such as hardness, thickness uniformity, weight fluctuation, and surface pH were assessed on the produced tablets. The bioadhesive strength and in-vitro drug release of the produced tablets were also tested. In vitro bioadhesive strength and release tests revealed that formulation F2, which had individual polymer and medication, had the best drug release (97.51%) and bioadhesive strength. The FTIR measurements revealed no evidence of interaction between polymer and drug.

Keywords: - Pioglitazone Hydrochloride, Bioadhesion, HPMC K4M, HPMC K15M, Carbopol 934P, Sodium Alginate.

# Introduction: -

Buccal drug delivery is a compelling alternative to oral medication administration, especially in terms of resolving the drawbacks of the latter. By giving the medicine via buccal route, problems like first pass metabolism and drug degradation in the GIT can be avoided. Furthermore, the oral cavity is conveniently accessible for self-medication, and toxicity can be quickly eliminated by removing the dose form from the buccal cavity. <sup>(8)</sup> This method can also be used to give drugs to people who are unable to take them orally. At least three of the following are required for successful buccal medication administration using a buccal adhesive system: (a) a bioadhesive to keep the system in the mouth cavity and optimise the amount of intimate contact with the drug; (b) a buccal adhesive system to keep the mucosa (b) a vehicle for releasing the medicine at an acceptable rate under the conditions in the mouth, and (c) techniques for overcoming the oral mucosa's limited permeability. Buccal adhesive drug delivery stems extend the duration spent in the mouth and operate as controlled-release dosage forms. <sup>(26, 27)</sup> Because the buccal mucosa is less permeable than the sublingual mucosa, it is a better candidate for extended drug administration. <sup>(47)</sup> Furthermore, the medicine is very well tolerated, and it can be applied, targeted, and removed at any moment during the treatment period. Due to the shorter half-life of pioglitazone hydrochloride, it is advantageous to solve the

problem of frequent dosage (3-5 h). Continual release of the increased bioavailability of the medicine results in a significant reduction in the dose and, as a result, dose-related side effects. <sup>(22,25)</sup> As a result, the current study attempted to manufacture a mucoadhesive buccal tablet for Pioglitazone hydrochloride utilising several polymer mixes in order to avoid substantial first-pass metabolism, stomach degradation, and the potentially fatal side effect of liver damage. <sup>(31,32)</sup>

# Materials and Method: -

# Materials

USV Private Limited, Mumbai, provided a free sample of pioglitazone hydrochloride. Colorcon, Goa, provided a free sample of Hydroxy Propyl Methyl Cellulose K15M, Hydroxy Propyl Methyl Cellulose K4M. Loba Chemicals in Mumbai, provided Sodium alginate and Carbopol 934. All of the other reagents were of analytical grade.

# Methods

# Selection of Active Pharmaceutical Agent

Pioglitazone hydrochloride is the hydrochloride salt version of the drug. It belongs to the thiazolidinediones class of drugs that reduce blood sugar levels. It can be used alone or in combination with other medications to treat type 2 diabetes. It enhances insulin sensitivity in muscle and adipose tissue and inhibits hepatic gluconeogenesis, as well as improving glycemic management and lowering insulin levels in the blood. It works by restoring the body's insulin sensitivity, a common hormone that helps maintain blood sugar levels.

# Formulation of Mucoadhesive Buccal Tablets

In a glass mortar, the drug, polymers, and excipients were homogeneously combined for 15 minutes. The combination (250 mg) was then compacted in a single stroke using a 9 mm biconcave punch on a station rotary machine (The Rimek Mini Press-1).

Ingredient's				-	Formu	lation	Code	U		
	<b>F1</b>	<b>F2</b>	<b>F3</b>	<b>F4</b>	<b>F5</b>	<b>F6</b>	F7	<b>F8</b>	F9	F10
Pioglitazone	30	30	30	30	30	30	30	30	30	30
HC1										
HPMC K15 M	100	-	-	-	50	-	-	50	50	-
HPMC K4M	-	100	-	-	50	50	-	-	-	50
Carbapol	-	-	100	-	-	50	50	50	-	-
Sodium	-	-	-	100	-	-	50	-	50	50
alginate										
Mannitol	100	100	100	100	100	100	100	100	100	100
Menthol	5	5	5	5	5	5	5	5	5	5
Disodium	5	5	5	5	5	5	5	5	5	5
saccharin										
Talc	5	5	5	5	5	5	5	5	5	5
Magnesium	5	5	5	5	5	5	5	5	5	5
stearate										

# Formula for the preparation of pioglitazone hydrochloride bucco-adhesive tablets.

# **EVALUATION OF BUCCO-ADHESIVE TABLET**

# DRUG AND POLYMER COMPATIBILITY STUDIES

An infrared spectrophotometer was used to record the drug's FTIR spectrum (Shimadzu Affinity-1). In the frequency range of 400-4000 cm-1, the IR spectrum of the medication, polymers, and their physical combination was recorded. The observed peaks were then logged and compared to the drug's standard FTIR.

# CALIBRATION CURVE OF PIOGLITAZONE HCL IN 6.8 PHOSPHATE BUFFER

10 mg of Pioglitazone HCl was dissolved in a tiny amount of phosphate buffer (pH 6.8) and used to make a volume of 100ml. To acquire solutions in the conc., repeated dilutions of the stock solution were performed. The concentrations range from 2 to 20 g/ml. A UV-visible spectrophotometer was used to test the solution's absorbance at 242 nm. Conc. V/s absorbance was displayed on a graph.

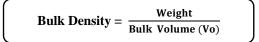
# CALIBRATION CURVE FOR PIOGLITAZONE HCL IN 7.4 PHOSPHATE BUFFER

The same was used to dilute 10 mg of Pioglitazone HCl in a little amount of phosphate buffer (pH 7.4) and make up to 100ml. To acquire solutions in the conc., repeated dilutions of the stock solution were performed. The concentrations range from 2 to 20 g/ml. A UV-visible spectrophotometer was used to test the solution's absorbance at 274 nm. Conc. V/s absorbance was displayed on a graph.

# PRECOMPRESSION STUDY

Angle of Repose - On rotation, the angle of repose is the greatest angle formed by the powder plane with the horizontal surface. Angle of repose is useful in determining particle flow parameters, which may be linked to packing densities and particle mechanical arrangements. Fixing the funnel and free-standing cone method was used to estimate the angle of powder repose. The granules were taken after being properly weighed. The funnel's height was then modified so that the funnel's tip just touched the granules' peak. Granules were permitted to freely flow through the funnel onto the surfaces. The powder cone's diameter and angle of repose were measured.

**Determination of Bulk density** – The volume and weight of preserved bulk powder can be measured and the apparent bulk density assessed by pouring it into a graduated measuring cylinder using a big funnel. The following formula is used to calculate bulk density:



Where, Vo-Bulk Volume

**Determination of Tapped density -** The volume and weight of preserved powder can be measured by putting it into a graduated measuring cylinder with a big funnel and tapping it 100 times on a wooden plank. The following formula can be used to determine tapped density.

Tapped Density = Weight Tapped Volume (Vt) Where, Vt-Tapped Volume

**Compressibility Index (or) Carr' index (I)** – Carr devised an indirect method of determining powder flow from bulk densities. Compressibility percentages are a direct indicator of the powder's potential arch and stability. The Carr's index of each prepared formulation was calculated.

**Hausner's ratio** – The ratio between tapped density and bulk density is used to calculate Hausner's ratio, which reveals the flow qualities of the powder. This ratio was shown to be related to inter particle friction by Hausner and could thus be used to predict powder flow parameters.

## POST COMPRESSION STUDY

## Thickness

Using a Digital Thickness Tester, the thickness of three randomly selected tablets from each formulation was measured in millimetres.

## **Weight Variation Test**

Twenty tablets are chosen at random and weighed individually in a single pan electronic balance, with the average weight determined. According to IP, no more than two individual weights should differ by more than 5% from the average weight, and none should differ by more than twice that percentage.

#### Hardness Test

The tablet was held between two jaws, one fixed and the other movable. The scale was set to zero, and the load was steadily increased until the tablet broke. The hardness of the tablet is determined by the load at that moment. For the hardness test, three tablets from each batch are utilised, and the findings are given in Kg/cm2.

# **Friability Test**

20 pre-weighed tablet samples are inserted in the friabilator, which is subsequently turned 100 times (4 min). After that, the tablets are dusted and reweighed. Compressed tablets with a weight loss of less than 0.5 to 1.0 percent are generally regarded as acceptable.

# **Determination of Drug Content**

Ten tablets are weighed and then crushed in a mortar to make powder. In a 100 ml volumetric flask, a quantity of powder weighing equivalent to 10 mg of medication was introduced, along with 6.8 Phosphate buffer. The solution is filtered using a membrane filter (0.45m), and 10 ml of the filtrate is transferred to a 100 ml volumetric flask, where 6.8 phosphate buffer is added to make up the final volume. The absorbance is then measured using a UV Visible spectrometer at 242 nm. The total amount of medication in a single tablet is then computed.

# Surface pH

The pH of the buccal tablets' surroundings (surface pH) was measured to see if there were any negative effects from the pH change in vivo. Because an acidic or alkaline pH can irritate the buccal mucosa, keeping the surface pH as close to neutral as possible was decided. For this, a composite glass electrode was used. The pill was allowed to swell for 2 hours at room temperature after being in contact with 5 mL of distilled

water (pH 6.5 0.05). The pH was determined by placing the electrode on the tablet surface and allowing it to equilibrate for 1 minute.

## **Mucoadhesive Strength**

A modified physical balance was used to assess the tablet's muco-adhesive strength. The fresh goat buccal mucosa was obtained from a local slaughterhouse and used within 2 hours of the animal's death. Phosphate buffer pH 6.8 and cut into a 3 cm piece An inverted 50ml beaker was placed in the centre of a 250ml beaker containing phosphate buffer, and a piece of buccal mucosa was stuck on it (pH 6.8). A cyanoacrylate adhesive was used to stick the tablet to the lower side of the glass vial. With a 5 gm weight on the right-hand side pan of the balance, two pans were balanced. The right-hand side pan was lowered along with the tablet over the mucosa after a 5 gram weight was removed from it. The For a total of 5 minutes, the balance was held in this position. Water was introduced to the right-hand side pan gently (100 drops/min.) until the patch separated from the mucosal surface. The muco-adhesive strength was determined by the weight in grammes required to remove the tablet from the mucosal surfaces. The weight required to separate the pill from the mucosal surface (goat buccal mucosa) is used to determine muco-adhesive strength. The muco-adhesive strength was used to compute the following parameters.

#### Force of adhesion (N) = (Bioadhesive strength/1000) $\times$ 9.81

#### *IN - VITRO* DRUG RELEASE STUDIES

The USP Type II (paddle) dissolution test Apparatus was used to test the dissolution characteristics of the prepared bucco-adhesive tablets of Pioglitazone hydrochloride for 8 hours.

**Method:** The dissolution vessel was filled with 500 mL of 6.8 phosphate buffer, and the medium temperature was set to 37°C 0.5°C. Each dissolution tank contains one tablet from a different batch, with the paddle rotating at 50 rpm. For up to 8 hours, 10 ml of sample is removed at predetermined intervals of one hour and replaced with the same volume of new medium. In a volumetric flask, the removed material is diluted to 10 mL and filtered using a 0.45 membrane filter. The drug content of the resulting samples is determined using a UV-Visible spectrophotometer at 242 nm.

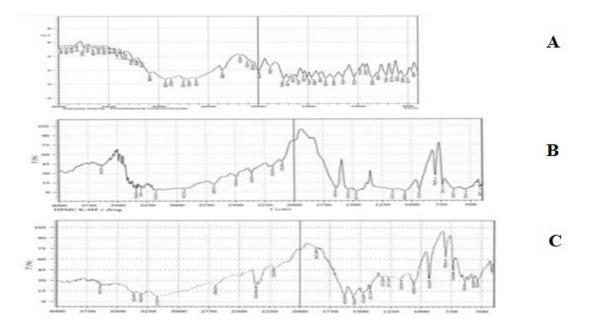
#### DETERMINATION OF SWELLING INDEX

One tablet was weighed and placed in a beaker containing 200 ml of medium for each formulation batch. The tablet should be taken from the media after each interval and weighed again for up to 8 hours, with the results recorded.

#### **RESULTS AND DISCUSSION**

#### EVALUATION OF BUCCO-ADHESIVE TABLET

#### Drug and polymer compatibility studies



Graph no. 1 – FTIR of Pioglitazone Hydrochloride and physical mixtures with polymers

- A FTIR of Pioglitazone Hydrochloride
- B FTIR of Pioglitazone Hydrochloride + HPMC K4M.
- C FTIR of Pioglitazone Hydrochloride + HHPMC K15M.

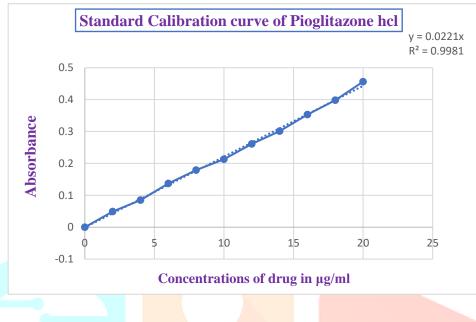
The results of FTIR study shows that, the drug was not found to show any interactions with the polymers i.e., HPMC K4M. and HPMC K15M. Hence, we can use the chosen polymers for further study.

#### CALIBRATION CURVE OF PIOGLITAZONE HCL IN 6.8 PHOSPHATE BUFFER

Concentrations (µg/mL)	Absorbance
0	0
2	0.049
4	0.085
6	0.137
8	0.179
10	0.213
12	0.261
14	0.301

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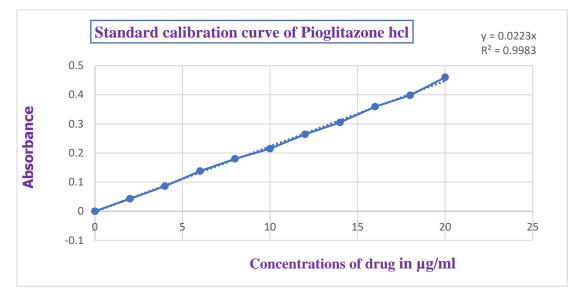
16	0.353
18	0.398
20	0.456

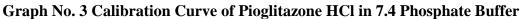


# Graph No. 2 Calibration Curve of Pioglitazone Hcl In 6.8 Phosphate Buffer

# CALIBRATION CURVE FOR PIOGLITAZONE HCL IN 7.4 PHOSPHATE BUFFER

Conc	entrations	Absorbance
(µg/n	nL)	
0		0
2		0.043
4		0.086
6		0.138
8		0.18
10		0.215
12		0.264
14		0.305
16		0.359
18		0.398
20		0.46





The calibration curve of Pioglitazone HCl shows the  $R^2$  value which is equal to 0.9995 nearly a straight line which shows that the study follows beerlaw.

#### PRECOMPRESSION STUDY

Ba	tch	Bulk Density	Tapped	Carr's Index	Hausner's	Angle of
		$(g/cm^3 \pm SD)$	Density (g/cm <sup>3</sup>	$(\% \pm SD)$	Ratio (± SD)	Repose
			± SD)			$(\theta \pm SD)$
F1		$0.460 \pm 0.002$	$0.525 \pm 0.010$	$12.52 \pm 0.78$	$1.14 \pm 0.05$	$31.25 \pm 1.17$
					6	
F2		$0.458 \pm 0.008$	$0.520 \pm 0.009$	$12.24 \pm 0.96$	1.14 ± 0.04	$31.40 \pm 1.09$
F3		$0.465 \pm 0.005$	$0.544 \pm 0.021$	$14.39 \pm 0.71$	$1.16 \pm 0.05$	$32.59 \pm 1.46$
F4		$0.450 \pm 0.012$	$0.515 \pm 0.024$	$12.32 \pm 0.75$	$1.14 \pm 0.03$	$31.41 \pm 1.18$
		0.451 0.005	0.500 0.000	12 10 0 00	1.1.5 0.0.5	21.54 1.22
F5		$0.451 \pm 0.006$	$0.522 \pm 0.009$	$13.10 \pm 0.68$	$1.15 \pm 0.02$	$31.56 \pm 1.23$
ГС		0.440 + 0.011	0.510 + 0.022	12.77 . 0.56	1.16 - 0.05	20.15 + 1.41
F6		$0.440 \pm 0.011$	$0.518 \pm 0.023$	$13.77 \pm 0.56$	$1.16 \pm 0.05$	$32.15 \pm 1.41$
F7		$0.445 \pm 0.009$	$0.511 \pm 0.008$	$13.81 \pm 0.44$	$1.16 \pm 0.07$	31.58 ± 1.34
Г/		$0.443 \pm 0.009$	$0.311 \pm 0.008$	$13.01 \pm 0.44$	$1.10 \pm 0.07$	$51.30 \pm 1.34$
F8		$0.458 \pm 0.013$	$0.529 \pm 0.019$	$12.76 \pm 0.90$	$1.14 \pm 0.09$	$33.05 \pm 1.04$
1.0		$0.+30 \pm 0.013$	$0.527 \pm 0.019$	$12.70 \pm 0.70$	$1.14 \pm 0.07$	55.05 ± 1.04
F9		$0.465 \pm 0.005$	$0.538 \pm 0.012$	$12.17 \pm 0.84$	$1.13 \pm 0.08$	32.45 ± 1.19
_						
F10	)	$0.462 \pm 0.002$	$0.525 \pm 0.007$	13.71 ± 0.49	$1.15 \pm 0.03$	31.43 ± 1.20

Table no. 1 – Pre – compression study

n =3

## POST COMPRESSION STUDY

Batch	Wt.	Hardness	Diameter	Thickness	Friability	Drug
	variation	$(\pm SD)$	(± SD)	$(\pm SD)$	(± SD)	Content
	$(\pm SD)$					
F1	249.96±0.	5±0.051	9.013±0.156	2.730±0.010	0.36±0.0025	86.20±2.34
	598					
F2	249.81±0.	4.6±0.059	9.014±0.156	2.741±0.005	$0.40 \pm 0.0018$	93.81±1.45
	601					
F3	249.82±0.	4.6±0.058	9.014±0.156	2.745±0.018	0.52±0.0019	91.48±143
	564					
F4	249.76±0.	5±0.054	9.014±0.156	2.752±0.013	0.36±0.0025	83.68±1.43
	578					
F5	249.87±0.	5±0.055	9.013±0.156	2.744±0.011	0.38±0.0021	91.46±1.46
	503					
F6	250.56±0.	4.8±0.05 <mark>9</mark>	9.014±0.156	2.739±0.008	0.41±0.0025	91.13±086
	616					
F7	249.78±0.	5±0.057	9.014±0.156	2.748±0.017	0.40±0.0018	90.57±067
	548					
F8	249.43±0.	4.8±0.05 <mark>5</mark>	9.013±0.156	2.752±0.015	0.39±0.0017	88.72±1.54
	532					
F9	250.12±0.	5.16±0.0 <mark>5</mark>	9.013±0.156	2.748±0.019	0.42±0.009	91.03±1.38
	628					
F10	250.21±0.	5.12±0.05	9.013±0.156	2.745±0.018	0.36±0.0025	90.38±2.35
	637					
n = 3						

 Table no. 2 – Post–compression study.

The Average Weight of all Bucco-adhesive tablets within formulation was found to be uniform. This indicates uniform filling of the die cavity during tablet compression.

The **Hardness** of all Bucco-adhesive tablets was found to be in the range of 5±0.051to 5.12±0.05

kg/cm2. This ensures good mechanical strength.

The **Thickness** of all Bucco-adhesive tablets was found in the range of  $2.730\pm0.010$  to  $2..745\pm0.018$ mm. There were no marked variations in the thickness of all formulations indicating uniform behavior of powder throughout the compression process.

The **Friability** of all Bucco-adhesive tablets was found to be in the raof nge  $0.36\pm0.0025$  to  $0.36\pm0.0025$  which indicates the goflowabilityity.

The Drug Content of all formulations was found to be between 86.20±2.34

to 90.38±2.35. The values ensure good uniformity of drug content in the tablet.

#### **Bioadhesive Parameters**

Batch	Surface pH	Drug Content (%)	Mucoadhesive strength (gms)	Force of adhesion (N)
F1	6.68±0.13	86.20±2.34	08.52±0.76	0.08±0.1
F2	6.56±0.11	93.81±1.45	11.69±0.24	0.10±0.1
<b>F</b> 3	6.48±0.16	91.48±143	09.54±0.75	0.09±0,2
F4	6.44±0.13	83.68±1.43	08.96±0.88	0.08±0.1
F5	6.74±0.15	91.46±1.46	11.28±0.88	0.11±0.1
F6	7.3±0.22	91.13±086	04.13±0.30	0.04±0.2
F7	6.44±0.13	90.57±067	05.67±0.32	0.05±0.2
F8	6.34±0.18	88.72±1.54	08.0 <mark>2±0.8</mark> 5	0.07±0.1
F9	7.07±0.15	91.03±1.38	10.56±0.35	0.105±0.3
F10	6.40±0.15	90.38±2.35	14.21±0.71	0.14±0.2

#### Table no. 3. Surface pH, Mucoadhesive strength, Force of adhesion

# In- Vitro Drug Release Study

TIME	CUMULATIVE % DRUG RELEASE									
(HRS)	F1	F2	<b>F3</b>	F4	F5	<b>F6</b>	F7	F8	F9	F10
0	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$
1	11.53± 0.198	<b>13.846</b> ± 0.169	6.92± 0.165	<b>9.23</b> ± 0.191	11.53± 0.175	6.92± 0.198	16.15± 0.195	<b>20.76</b> ± 0.191	13.84± 0.188	9.23± 0.165
2	20.58± 0.185	<b>22.895</b> ± 0.199	<b>20.49</b> ± 0.178	<b>27.33</b> ± 0.175	25.11± 0.188	<b>20.49</b> ± 0.191	<b>34.25</b> ± 0.197	<b>34.34</b> ± 0.195	<b>20.63</b> ± 0.165	25.06± 0.178
3	<b>32.3</b> ± 0.191	<b>34.66</b> ± 0.181	<b>34.47</b> ± 0.191	<b>41.44</b> ± <b>0.</b> 184	<b>36.92</b> ± 0.176	<b>34.47</b> ± 0.195	48.5± 0.181	50.85± 0.197	<b>32.35</b> ± 0.176	43.66± 0.195
4	<b>44.25</b> ± 0.198	<b>48.914</b> ± 0.187	<b>48.73</b> ± 0.195	51.31± 0.189	<b>46.69</b> ± 0.198	<b>44.2</b> ± 0.178	60.76± 0.179	69.95± 0.191	<b>44.29</b> ± 0.188	58.09± 0.156

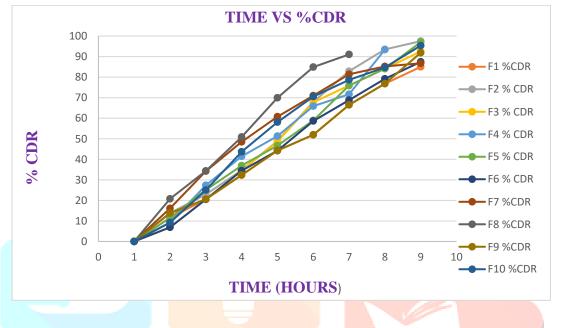
Table No. 4. In vitro drug release study

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5	51.9±	67.963±	67.78±	65.88±	58.91±	58.64±	70.99±	84.88±	51.94±	70.54±
	0.198	0.195	0.178	0.175	0.191	0.185	0.156	0.181	0.185	0.189
6	66.47±	82.85±	75.88±	71.67±	75.88±	68.82±	81.4±	91.04±	66.51±	78.68±
	0.179	0.173	0.199	0.165	0.195	0.198	0.186	0.176	0.196	0.179
7	76.78 ±	93.484±	84.11±	93.39±	84.11±	79.18±	85.2±		76.83±	84.7±
	0.177	0.189	0.181	0.159	0.165	0.169	0.169		0.185	0.191
8	85.02±	97.511±	92.48±		97.01±	87.46±	86.78±		91.85±	95.33±
	0.165	0.189	0.177		0.177	0.191	0.188		0.195	0.177

n=3



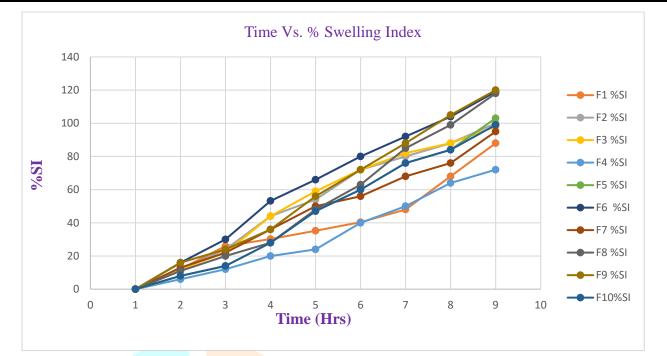
Graph No. 4 Time Vs. % CDR

# DETERMINATION OF SWELLING INDEX

	Table no.	$5 - \frac{9}{2}$	o Swel	ling Index
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Time	F1 ± SD	$F2 \pm SD$	F3 ± SD	F4 ± SD	F5±SD	F6 ± SD	F7 ± SD	F8 ± SD	F9± SD	F10±SD
Time	FT ± SD	r2±5D	F5 ± 5D	ITT 1 SD	F5±5D	FU I SD	F7±SD	10 - 30	FJ± SD	T 10±5D
0	$0\pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0 \pm 0$	$0\pm 0$	$0 \pm 0$	$0\pm 0$	$0\pm 0$
1	12 ±	12 ±	12 ±	$6 \pm 0.895$	8 ±	16 ±	13 ±	11 ±	16 ±	8 ±
	0.895	0.895	0.895		0.895	0.895	0.895	0.895	0.895	0.895
2	26 ±	24 ±	22 ±	12 ±	14 ±	30 ±	22 ±	20 ±	24 ±	14 ±
	0.605	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895
3	30.2 ±	44 ±	44 ±	20 ±	28 ±	53.2 ±	36 ±	28 ±	36 ±	$28 \pm$
	0.712	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895
4	35.2 ±	54 ±	59 ±	24 ±	47.2 ±	66 ±	50 ±	48 ±	56 ±	47 ±
	0.887	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895
5	40.4 ±	72 ±	72 ±	40 ±	60 ±	80 ±	56 ±	63 ±	72 ±	60 ±
	0.568	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895
6	48.4 ±	80 ±	82 ±	50 ±	76 ±	92 ±	68 ±	85 ±	88 ±	76 ±
	0.897	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895
7	68 ±	88 ±	88 ±	64 ±	84 ±	104 ±	76 ±	99 ±	105 ±	84 ±
	0.689	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895
8	88 ±	100 ±	1 ±	72 ±	103 ±	119 ±	95 ±	118 ±	120 ±	99 ±
	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895	0.895

n=3



Graph No. 5 % SI Index

# CONCLUSION

The literature review on the buccal drug delivery technique suggests that it is effective for medicines with low molecular weight, low dosage, and considerable first-pass metabolism. Pioglitazone hydrochloride is an anti-diabetic medication with low molecular weight, low dose, strong biphasic solubility, and substantial first-pass metabolism, making it a good candidate for use in the buccal mucoadhesive drug delivery method. A review of the literature on HPMC, carbopol, and chitosan polymers found that they exhibit strong bioadhesive characteristics. The FT-IR validated the purity of the medication. The medicine and the polymers did not interact in any way. HPMC K4M, HPMC K15M, Carbopol, and Sodium alginate in various amounts were used to make buccoadhesive tablets containing pioglitazone hydrochloride.

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