



DESIGN AND DEVELOPMENT OF BILAYER TABLET OF ETORICOXIB AND ETODOLAC

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Abstract

Objective

The main goals of the current study were to improve patient compliance and develop a two-layer drug delivery system that would allow for drug release at a predetermined time following an initial release. This would allow for sustained drug release from the formulation during the effective treatment of arthritis. Increasing the bioavailability of etodolac and etoricoxib was the aim of the current investigation.

Methods

An immediate release layer and a sustain release layer made up the two distinct components of the created Biayer drug delivery system. Crosspovidone was included in the immediate release layer together with the active component as a super disintegrant. Using the wet granulation process, the tablet was made. Kolloidon SR was used as a release-delaying polymer in the sustained release layer. Sustain release layer preparation was done using the direct compression method.

Result

The developed formulations were assessed for their in vitro drug release profile, in vitro disintegration time, and physical properties.

Conclusion

On the basis of these evaluation shown that optimized bilayer tablets formulation F5 showed 12 hrs drug release of Etodolac and F8 showed disintegration time is 36 sec for immediate release. The bilayer formulation by factorial showed compliance with treatment of Arthritis.

Key Words: Etodolac, Etoricoxib, Crosspovidone, Kollidion SR, Bilayer Tablet

Introduction

The oral route of drug administration stands out as the most significant and convenient method for delivering medications. However, the potential for sustained drug release over extended periods hasn't been fully tapped due to variations in absorption across different sections of the gastrointestinal tract (GIT). Consequently, only a handful of drug delivery systems have been developed to target specific regions of the GIT, such as the stomach, upper small intestine, or colon.

Worldwide, the two most prevalent conditions are joint pain (which includes back pain) and arthritis (which includes rheumatoid arthritis and osteoarthritis). Around 350 million episodes of arthritis-related knee pain occur worldwide each year, making it the second most feared condition after cardiovascular disease.

Encouraging patient convenience and compliance, the pharmaceutical industry has been more interested in the past ten years in developing a combination of two or more API in a single dosage form (bilayer tablet). When developing distinct drug release profiles (immediate release with extended release), bilayer tablets might be a major option to prevent chemical incompatibilities across API by physical separation. There are several major benefits of bilayer tablets. in reference to traditional monolayer tablets.

Bilayer tablets are a better option since one layer delivers the medication instantly, and the controlled release layer of the tablet keeps the drug's plasma level stable. The more recent and effective method for developing controlled release for emulsion is the bilayer tablet, which is superior to the dosage forms that have been employed in the past. Bilayer tablets are useful for the sequential release of two medications in combination. They can also be used for sustained release, where one layer is used for immediate release as the inceptive dose and the second layer is used as the maintenance dose.

Materials and methods

Etodolac was obtained from A.R. Life science Pvt. Ltd. Etoricoxib was obtained from Assurgen pharma pvt. Ltd. Avicel 101 as a diluent obtained from Patel chem. Specialist Ahemdabad, Filler lactose, starch also Binder PVP K 30 obtained from S.D. Fine chemicals Ahemdabad, Polymer Koloidn SR was obtained from global life science pvt, ltd. Superdisintigrant Crosspovidone was obtained from Vasa pharma chem.. Ahemdabad. Talc and Magnesium Stearate as a glidant and lubricant was obtained from Patel chemicals, Ahemdabad and Gangotri inorganics, pvt, ltd. Ahemdabad.

Method of Preparation of Bilayer Tablets

The preliminary trials for polymer selection involved preparing tablets using different matrix-forming agents via wet granulation technique. In these preparation two layer were selected. 1) Immediate release layer and 2) Sustained release layer. In these preparation first of all Blends comprising the drug, diluents, and sustained release polymer were thoroughly mixed after passing through a 40# sieve. Then its bind using the binder like PVP k 30 solution. After completion of granulation process the bulk were dried and its passed through sieve no.22#. Talc and magnesium stearate were then added as glidant and lubricant, respectively. The blend was compressed using a bilayer tablet compress machine.

Table 1 Formulation Table of Trial Batches of Immediate release layer tablets

Ingredients (mg)	TF1	TF2	TF3	TF4	TF5	TF6	TF7	TF8	TF9
Etoricoxib	60	60	60	60	60	60	60	60	60
MCC 101	51	46	41	51	46	41	51	46	41
Lactose	115	115	115	115	115	115	115	115	115
Starch	6	6	6	6	6	6	6	6	6
SSG	5	10	15	-	-	-	-	-	-
CCS	-	-	-	5	10	15	-	-	-
Crosspovidone	-	-	-	-	-	-	5	10	15
MagnesiumStearate	4	4	4	4	4	4	4	4	4
Talc	6	6	6	6	6	6	6	6	6
Aerosil	3	3	3	3	3	3	3	3	3
Total (mg)	250	250	250	250	250	250	250	250	250

Table 2 Formulation Table of Trial Batches of Sustained release layer tablets

Ingredients (mg)	TS1	TS2	TS3	TS4	TS5	TS6	TS7	TS8	TS9
Etodolac	400	400	400	400	400	400	400	400	400
MCC 101	70	70	70	70	70	70	70	70	70
Lactose	50	40	30	50	40	30	50	40	30
PVP K 30	12	12	12	12	12	12	12	12	12
Ethyl cellulose	50	60	70	-	-	-	-	-	-
Kolloidon SR	-	-	-	50	60	70	-	-	-
HPMC K4M	-	-	-	-	-	-	50	60	70
Magnesium Stearate	8	8	8	8	8	8	8	8	8
Talc	10	10	10	10	10	10	10	10	10
Total (mg)	600	600	600	600	600	600	600	600	600

Table 3 Layout of Factorial Design of Immediate release layer

3 ² Full Factorial Designs			
Batch No.	X1 Amount of Lactose	X2 Superdisintegrant Crosspovidone	
FIR1	-1	-1	
FIR2	-1	0	
FIR3	-1	+1	
FIR4	0	-1	
FIR5	0	0	
FIR6	0	+1	
FIR7	+1	-1	
FIR8	+1	0	
FIR9	+1	+1	
Translation of coded level in actual limit			
Independent variables	Real Value		
	Low(-1)	Medium(0)	High(+1)
Amount of lactose (mg) X1	110	115	120
Superdisintegrant crosspovidone (mg) X2	7.5	12.5	17.5

- **Input variables**
 - ✓ X1-Amount of Lactose in (mg)
 - ✓ X2-Crosspovidone dosage (mg)
- **Output variables**
 - ✓ Y1- % Drug release at 1 hour
 - ✓ Y1- Disintegration time

Table 4 Layout of Factorial Design of Sustained release layer

3 ² Full Factorial Designs		
Batch No.	X1 Amount of PVP K 30	X2 Amount of Kolloidon SR
FSR1	-1	-1
FSR2	-1	0
FSR3	-1	+1
FSR4	0	-1
FSR5	0	0
FSR6	0	+1
FSR7	+1	-1
FSR8	+1	0

FSR9	+1	+1
Translation of coded level in actual limit		
Independent variables	Real Value	
	Low(-1)	Medium(0)
Amount of PVP K 30 X1(%)	2	3
Amount of X2 Kolloidon SR X2 (%)	8	12

- **Independent variables**
 - ✓ X₁-Amount of PVP K 30 (%)
 - ✓ X₂-Amount of Kolloidin SR (%)
- **Dependent variables**
 - ✓ Y₁- % Drug release at 1 hour
 - ✓ Y₁- Hardness

Table 5 Formulation Table of Factorial Batches of Immediate release layer tablets

Ingredients (mg)	F1	F2	F3	F4	F5	F6	F7	F8	F9
Etoricoxib	60	60	60	60	60	60	60	60	60
MCC 101	53.5	48.5	43.5	48.5	43.5	38.5	43.5	38.5	33.5
Lactose	110	110	110	115	115	115	120	120	120
Starch	6	6	6	6	6	6	6	6	6
Crosspovidone	7.5	12.5	17.5	7.5	12.5	17.5	7.5	12.5	17.5
Magnesium Stearate	4	4	4	4	4	4	4	4	4
Talc	6	6	6	6	6	6	6	6	6
Aerosil	3	3	3	3	3	3	3	3	3
Total (mg)	250	250	250	250	250	250	250	250	250
Etoricoxib	60	60	60	60	60	60	60	60	60

Table 6 Formulation Table of Factorial Batches of Sustained release layer tablets

Ingredients (mg)	F1	F2	F3	F4	F5	F6	F7	F8	F9
Etodolac	400	400	400	400	400	400	400	400	400
MCC 101	60	60	60	60	60	60	60	60	60
Lactose	62	50	38	59	47	35	56	44	32
PVP K 30	12	12	12	15	15	15	18	18	18
KolloidonSR	48	60	72	48	60	72	48	60	72
Magnesiumstearate	8	8	8	8	8	8	8	8	8
Talc	10	10	10	10	10	10	10	10	10
Total (mg)	600	600	600	600	600	600	600	600	600
Etodolac	400	400	400	400	400	400	400	400	400
MCC 101	60	60	60	60	60	60	60	60	60

Methodology

Preformulation

Characterization of API: -

Organoleptic property:

This involves documenting the drug's hue and scent using precise language. and record the same in results and discussion chapter.

Flow Property:

The study examined the flow characteristics of API/powder blends. To determine bulk density, 10 grams of powder were carefully poured into a 50-milliliter measuring cylinder without compaction, and the volume of the powder was recorded. After tapping the powder 100 times, the volume was measured to obtain the desired tapped density. The powder mixtures' Carr's index (CI) & Hausner ratio (HR) were calculated using the measurements of powder densities.

Melting point:

The Melting Point Testing Apparatus: technique was incorporated into the device to determine the drug's (API) melting point.

Using a modern melting point apparatus, the following steps are needed to measure melting point:

- make sure the sample is completely dry and powdered
- put the sample in a capillary tube
- insert the capillary tube to the melting point apparatus
- quickly heat the sample to a predetermined temperature
- slow down the rate of temperature increase to see when the sample melts
- view the melting point through a viewing eyepiece
- digitally record the melting point.

Drug Excipient Compatibility Study

FTIR investigations were conducted to evaluate the compatibility between excipients and the drug. Samples of the pure drug and physical mixtures of excipients with the drug were analyzed using FTIR to assess their compatibility. The distinctive peaks corresponding to various functional groups were compared with established standard peaks to determine any discrepancies.

Calibration Curve

Preparation of Standard Calibration Curve of Etoricoxib

Principle: The Etoricoxib exhibits peak absorbance at 233 nm in 0.1 N HCl (1.2 pH).

Instrument used: UV - Vis 1700 Spectroscopy by Shimadzu, UV Spectrophotometer, Japan.

Procedure:

- Preparation of standard solution : 100 mg of etoricoxib was precisely measured and dissolved in a small volume of 0.1 N HCl (pH 1.2) in a 100 ml volumetric flask. The solution was then diluted with 0.1 N HCl (pH 1.2) to achieve a concentration of 100 0 μ g/ml (SS-I). From this solution, 10 ml was withdrawn and further diluted to 100 ml to obtain a concentration of 100 μ g/ml (SS-II).
- Preparation of working standard solutions: Aliquots of 0.2 ml, 0.4 ml, 0.6 ml, 0.8 ml and 1 ml from SS-II were pipetted into 10 ml volumetric flasks. The volume was adjusted with 0.1 N HCl (pH 1.2) to achieve final concentrations of 2, 4, 6, 8, and 10 μ g/ml, respectively. The absorbance of each concentration was measured at 233 nm.
- A solution containing Etoricoxib (10 μ g/mL) from SS-II was scanned in the UV region to identify the wavelength.
- λ_{max} : 233 nm
- Beer's range: 2-10 μ g/ml.

Preparation of Standard Calibration Curve of Etodolac

Principle: The Etodolac exhibits peak absorbance at 276 nm in Phosphate buffer solution (6.8 pH).

Instrument used: UV - Vis 1700 Spectroscopy by Shimadzu, UV Spectrophotometer, Japan.

Procedure:

- Preparation of standard solution : 100 mg of Etodolac was precisely measured and dissolved in a small volume of Phosphate buffer (pH 6.8) in a 100 ml volumetric flask. The solution was then diluted with Phosphate buffer (pH 6.8) to achieve a concentration of 1000 µg/ml (SS-I). From this solution, 10 ml was withdrawn and further diluted to 100 ml to obtain a concentration of 100 µg/ml (SS-II).
- Preparation of working standard solutions: Aliquots of 0.2 ml, 0.4 ml, 0.6 ml, 0.8 ml and 1 ml from SS-II were pipetted into 10 ml volumetric flasks. The volume was adjusted with Phosphate buffer (pH 6.8) to achieve final concentrations of 2, 4, 6, 8, and 10 µg/ml, respectively. The absorbance of each concentration was measured at 276 nm.
- A solution containing Etodolac (10 µg/mL) from SS-II was scanned in the UV region to identify the wavelength.
- λ_{max} : 276 nm
- Beer's range: 2-10 µg/ml.

Evaluation Parameters of Tablets

(A) Pre compression Parameters: -

Bulk Density:

Computed using the formula that follows.

$$\text{Bulk density} = \text{Weight of powder} / \text{Bulk volume}$$

Tapped Density

Computed using the formula that follows

$$\text{Tapped density} = \text{Weight of powder} / \text{Tapped volume}$$

Compressibility Index (CI):

Computed using the formula that follows

$$\text{Carr's Compressibility index (\%)} = \{(TD - BD) / TD\} \times 100.$$

Table 7 Scale of flow ability by Compressibility index

C.I.	Category	Hausner's Ratio
<10	Excellent	1.00–1.110
11 – 15	Good	1.12–1.180
16 – 20	Fair	1.19–1.250
21 – 25	Passable	1.26–1.340
26 – 31	Poor	1.35–1.450
32 – 37	Very poor	1.46–1.590
>38	Very very poor	>1.600

Hausner's Ratio:

The formula below can be used to compute this.

$$\text{Hausner's ratio} = \text{Tapped density} / \text{Bulk density}$$

(B) Post Compression Parameters

Weight Variation

An electric digital balance was used to weigh twenty tablets of each formulation, and the average weight was determined.

Table 8 IP/BP/USP limit of weight variation test.

IP/BP Average weight of tablet (mg)	% Deviation	USP Average weight of tablet (mg)
130 or less	10.0	80 or less
From 130 to 324	7.5	From 80 to 250
More than 324	5.0	More than 250

Hardness

Hardness was assessed by diametrically compressing six tablets from each batch using a Monsanto hardness tester, and average values were subsequently computed.

Friability

Friability, which indicates tablet strength, was assessed using a Roche-type friabilator following this procedure: After twenty tablets were weighed precisely, they were put into the tumbling device, which turned at a speed of twenty-five revolutions per minute, lowering the tablets every six inches. The tablets were tumbling for four minutes, and a percentage of weight loss was computed by reweighing the tablets.

$$\% \text{ loss} = \frac{\text{initial wt.} - \text{final wt.}}{\text{initial wt.}} \times 100$$

Thickness

Using vernier callipers, the thickness of the buccal tablets was measured. A random selection of ten tablets was made from each batch. and their thickness was individually assessed. The average thickness was then calculated from the recorded measurements.

Assay

Ten tablets were individually weighed and then pulverized. Next, an amount of powder equivalent to one tablet was weighed, and the drug was extracted in 0.1 N HCl, and Phosphate buffer P^H 6.8. The resulting solution was filtered through a 0.45 µm membrane. After appropriate dilution, the absorbance was measured using a Shimadzu UV-1700 UV/Vis double-beam spectrophotometer.

In Vitro Dissolution Studies

Using USP apparatus II, the dissolution profile was investigated while the dissolution medium (900 ml of 0.1N HCl) was kept at 37°C ± 0.5°C at 50 rpm. Each batch of pills had six that were put into separate baskets with the HCl solution within. Over the course of 30 min , 10 ml samples were taken out every 5

minute. A filter was applied to these samples. These solutions' absorbance was determined using a UV spectrophotometer.

***In Vitro* Dissolution Studies**

Using USP apparatus II, the dissolution profile was investigated while the dissolution medium (900 ml of phosphate buffer P^H 6.8) was kept at 37°C ± 0.5°C at 50 rpm. Each batch of pills had six that were put into separate baskets with the phosphate buffer P^H 6.8 solution within. Over the course of 12 hours, 10 ml samples were taken out every hour. A filter was applied to these samples. These solutions' absorbance was determined using a UV spectrophotometer.

Drug Release Kinetic Study

The zero order, first order, Korshmer and Papps, and Higuchi equation models were among them. Plotting the obtained data using the following models allowed us to study the release kinetics: Higuchi's model (Equation 3), which shows the cumulative percentage of drug released against the square root of time; zero order, which represents cumulative drug release over time (Equation 1); and first order, which shows the log cumulative percentage of remaining drug versus time (Equation 2). Drugs dissolved from pharmaceutical formulations that release the drug gradually without disaggregation are described by zero order kinetics.

$$Q_1 = Q_0 + K_0 t \quad \dots\dots\dots 1$$

Q_0 is the starting concentration of drug in solution, Q_1 is the amount of drug dissolved at time t , and K_0 is the zero-order rate constant, given in concentration units over time. Hours of time are represented by the variable t . A concentration versus time plot graphed would connect the axes' origin and produce a straight line with a slope equal to K_0 . First order model has been used to describe absorption and elimination of drugs. The following equation express this model.

$$\text{Log } Q_1 = \text{Log } Q_0 + (K_1 t / 2.303) \dots\dots\dots 2$$

where Q_0 is the starting drug concentration in the solution, K_1 is the first order release constant, and Q_1 is the amount of drug released in time t . This will result in a linear graph showing the decimal logarithm of the amount of drug that has been released over time.

In order to investigate the release of pharmaceuticals that are water soluble and low solubility when incorporated into semi-solid or solid matrices, Higuchi created a number of models. Giving rise to the following expression.

$$Q = K_H t^{1/2} \quad \dots\dots\dots 3$$

where t is the time in hours, Q is the amount of drug released at time t , and K_H is the Higuchi dissolution constant reflecting the system's design characteristics. Therefore, the reciprocal of the square root of time and the medication release rate are proportionate. According to Higuchi, drug release is a diffusion mechanism that is time-dependent and based on Fick's law, square root.

Mechanism of Drug Release : Data from the dissolution research were plotted in Korsmeyer Peppas's equation as log cumulative percentage of drug released vs. log time in order to assess the mechanism of drug release from tablets. The exponent n was then determined by calculating the slope of the straight line.

$$F = (M_t / M) = K_m t^n \dots\dots\dots 4$$

where K_m is a constant dependent on the geometry of the dosage form, ' n ' is the slope of the linear plot, M_t is the drug release at time t , F is the fraction of drug release at time t , and M is the total amount of medication in the dosage form. The releasing mechanism is indicated by the value of n .

When the exponent value n is equal to 0.5 in Fickian diffusion, and when it is between 0.5 and 1.0 in non-Fickian diffusion, it is considered abnormal. When the exponent value is $n=1$, it denotes a standard zero-order release or Case-II Transport.

Stability Study

For a month, the optimised batch of floating tablets was subjected to accelerated stability testing in a humidity chamber with a temperature of 40°C and a relative humidity of 75%. The best batch of tablets were evaluated for appearance, drug content, floating qualities, and in vitro drug release characteristics before being wrapped in aluminium foil pouches.

Results & discussion

Preformulation Study of Etoricoxib drug

Table 9 API properties

Sr. No.	Characteristic Properties	Observation/Result	
1	Organoleptic Characteristics	Colour of API	It is White colour crystalline Powder
		Odour of API	It is Odourless powder
2	Flow Properties	Bulk density of API (g/ml)	0.836 ± 0.01
		Tapped density of API (g/ml)	1.253 ± 0.01
		Carr's index (%) of API	33.28 ± 0.02
		Hausner's ratio of API	1.49 ± 0.01
		Angle of repose (θ°) of API	38.6 ± 0.2
3	Solubility	It is soluble in organic solvents. Practically insoluble in water.	
4	Melting Point	135-136 °C	

Standard Calibration Curve of Etoricoxib

The standard calibration curve was prepared in 0.1 N HCl (pH 1.2). The λ_{\max} found 233 nm. Please refer below figure for λ_{\max} .

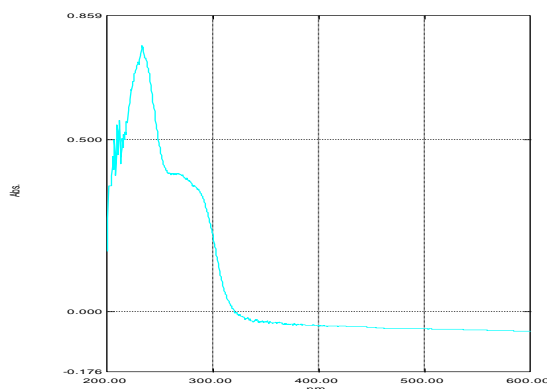


Figure 0-1 λ_{\max} of Etoricoxib in 0.1 N HCl

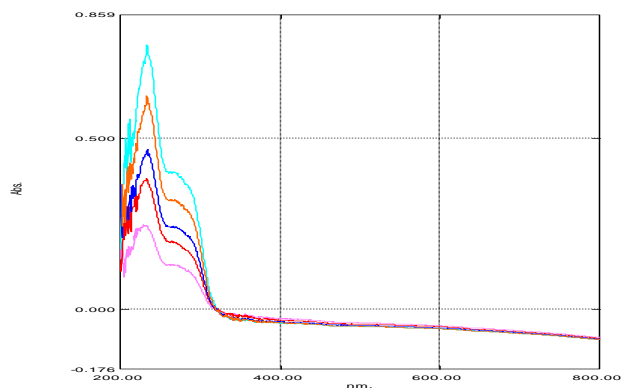


Figure 2 Overlay plot of Etoricoxib in 0.1 N HCl

Table 10 Standard calibration curve Etoricoxib in 0.1 N HCl

Concentration ($\mu\text{g/ml}$)	Absorbance (Average) \pm SD
0.0	0.0 \pm 0.000
2	0.251 \pm 0.002
4	0.379 \pm 0.004
6	0.472 \pm 0.003
8	0.626 \pm 0.006
10	0.786 \pm 0.002

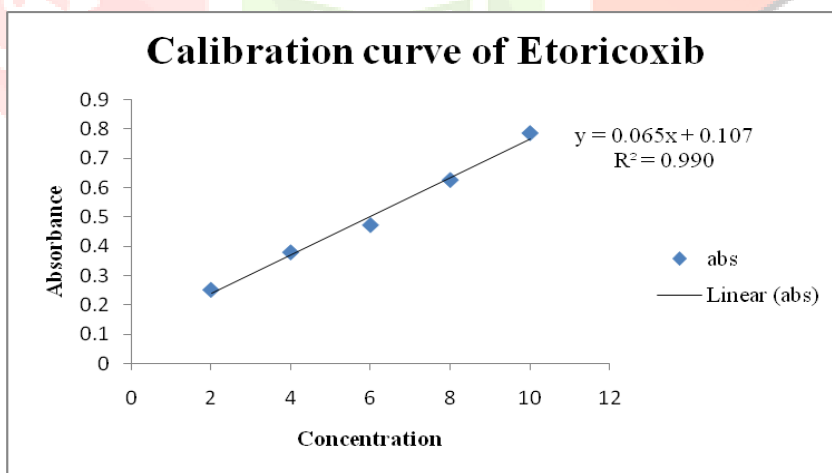


Figure 3 Calibration curve of Etoricoxib in 0.1 N HCl

Drug- excipient compatibility studies

The medication and some excipients were compatible, according to an FTIR investigation. There were no interactions of any type between the medication and the excipients. Please refer to figures.

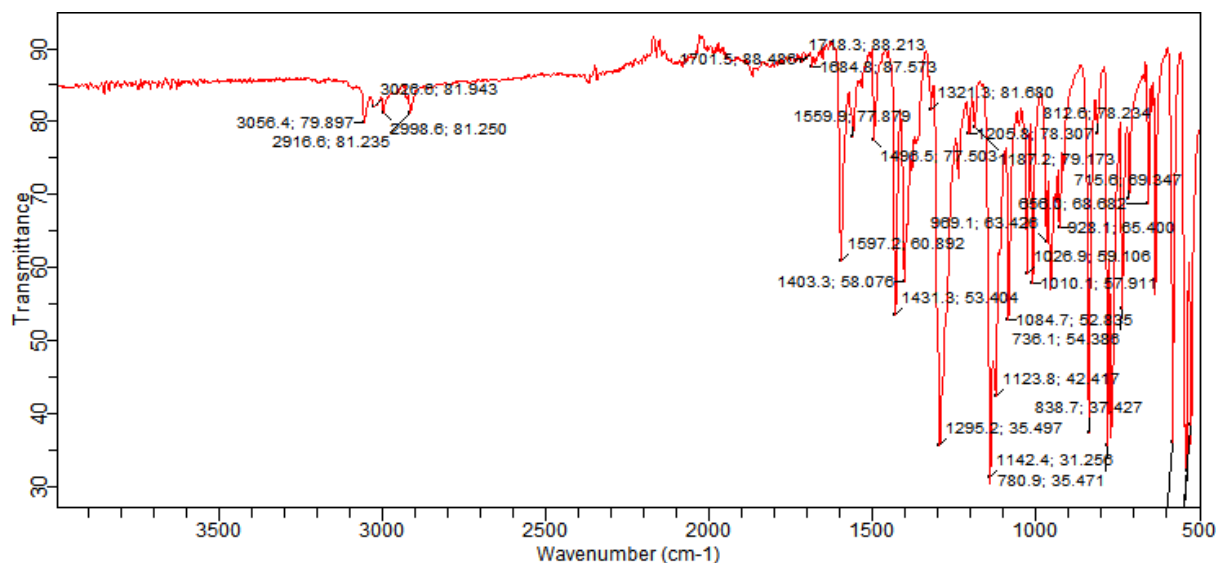


Figure 4 FTIR spectra of Etoricoxib

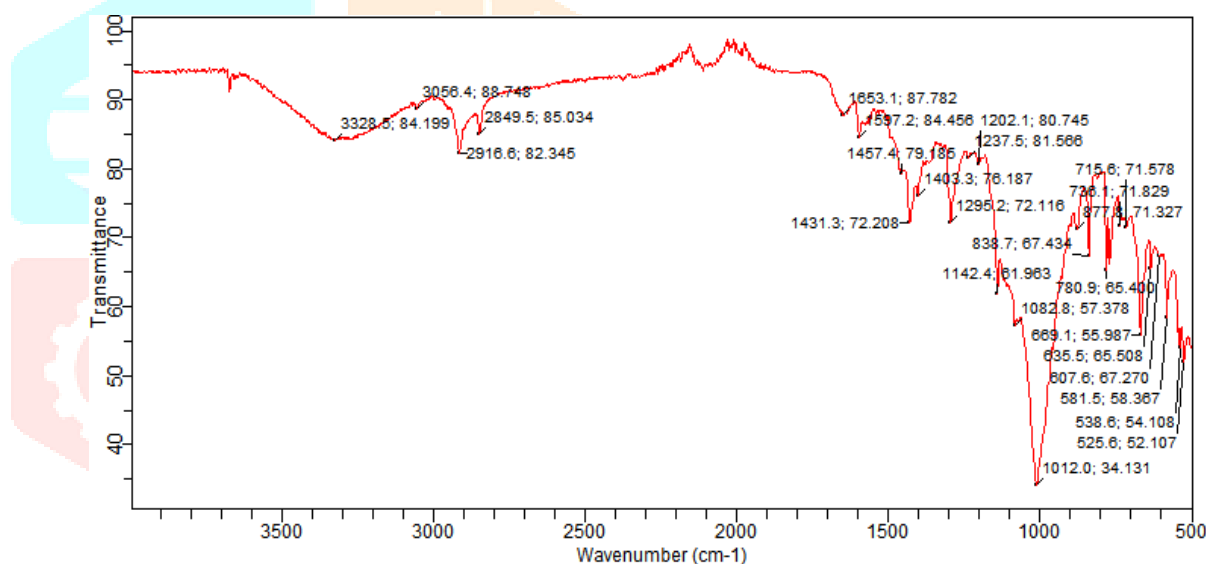


Figure 5 FTIR of Physical Mixture of Optimized Formulation

Table 11 Interaction studies through IR spectroscopy

Stretching	Etoricoxib	Formulation
	Peak cm ⁻¹	Peak cm ⁻¹
C=N	1597.2	1597.2
S=O	1431.3	1431.3
C-Cl	838.7	838.7

Conclusion: Based on the FTIR study findings presented above, it was concluded that there were no notable interactions observed between the drug and excipients. Therefore, the drug and other excipients are deemed compatible with each other.

Preformulation Study of Etodolac drug

Table 12 API properties

Sr. No.	Characteristic Properties		Observation/Result
1	Organoleptic Characteristics	Colour of API	It is White to off white Powder
		Odour of API	It is Odourless powder
2	Flow Properties	Bulk density of API (g/ml)	0.315 ± 0.03
		Tapped density of API (g/ml)	0.485 ± 0.01
		Carr's index (%) of API	33.05 ± 0.03
		Hausner's ratio of API	1.53 ± 0.01
		Angle of repose (θ°) of API	34.5 ± 0.2
3	Solubility	It is soluble in organic solvents. Practically insoluble in water.	
4	Melting Point	145-148 °C	

Standard Calibration Curve of Etodolac

The standard calibration curve was prepared in Phosphate buffer (pH 6.8). The λ_{\max} found 276 nm. Please refer below figure for λ_{\max} .

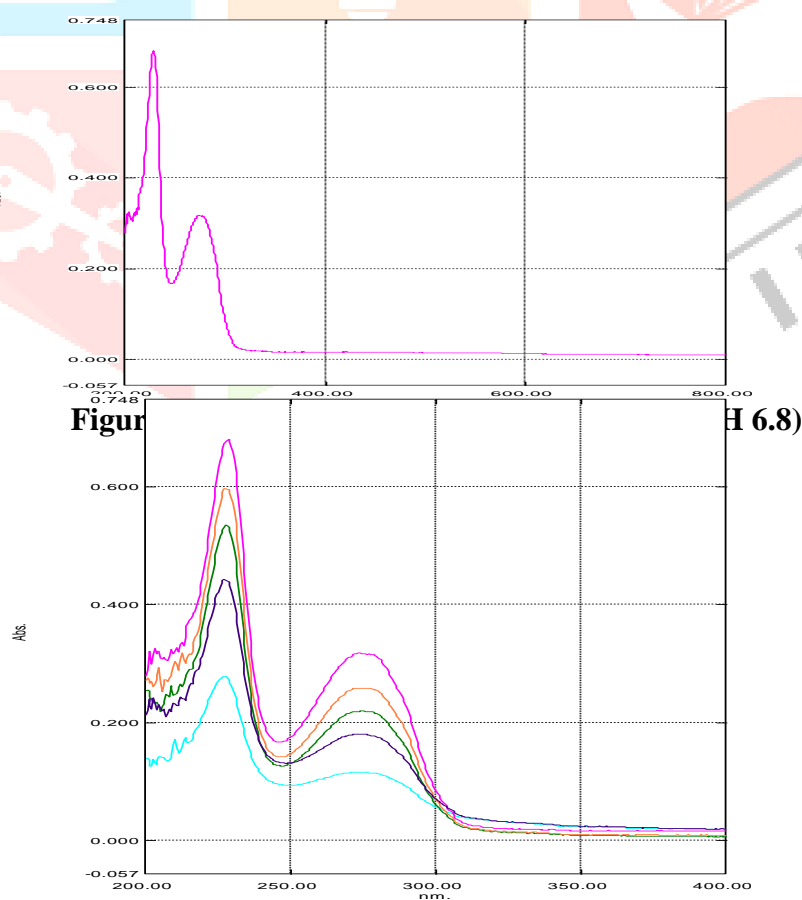
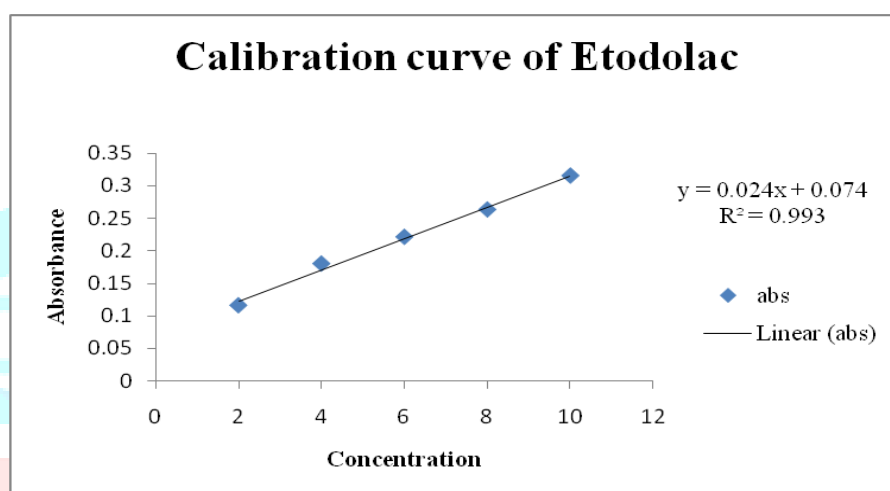


Figure 7 Overlay plot of Etodolac in Phosphate buffer (pH 6.8)

Table 13 Standard calibration curve Etodolac in Phosphate buffer (pH 6.8)

Concentration ($\mu\text{g/ml}$)	Absorbance (Average) \pm SD
0.0	0.0 \pm 0.000
2	0.116 \pm 0.004
4	0.183 \pm 0.004
6	0.221 \pm 0.003
8	0.263 \pm 0.004
10	0.315 \pm 0.002

Figure 8 Calibration curve of Etodolac in Phosphate buffer P^H 6.8

Drug- excipient compatibility studies

The medication and some excipients were compatible, according to an FTIR investigation. There were no interactions of any type between the medication and the excipients. Please refer to figures.

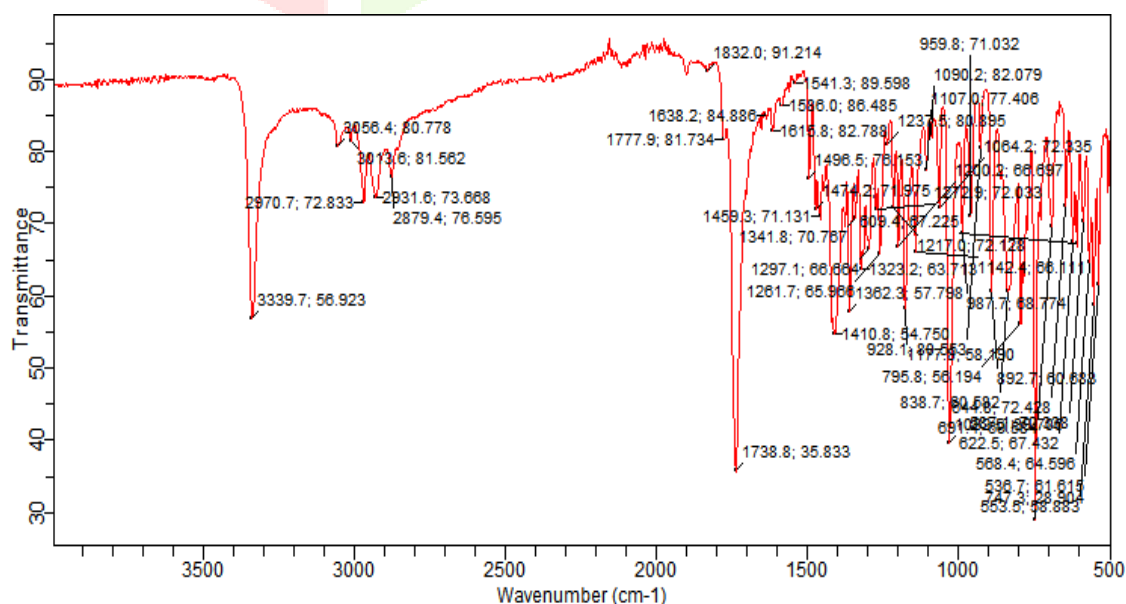


Figure 9 FTIR spectra of Etodolac

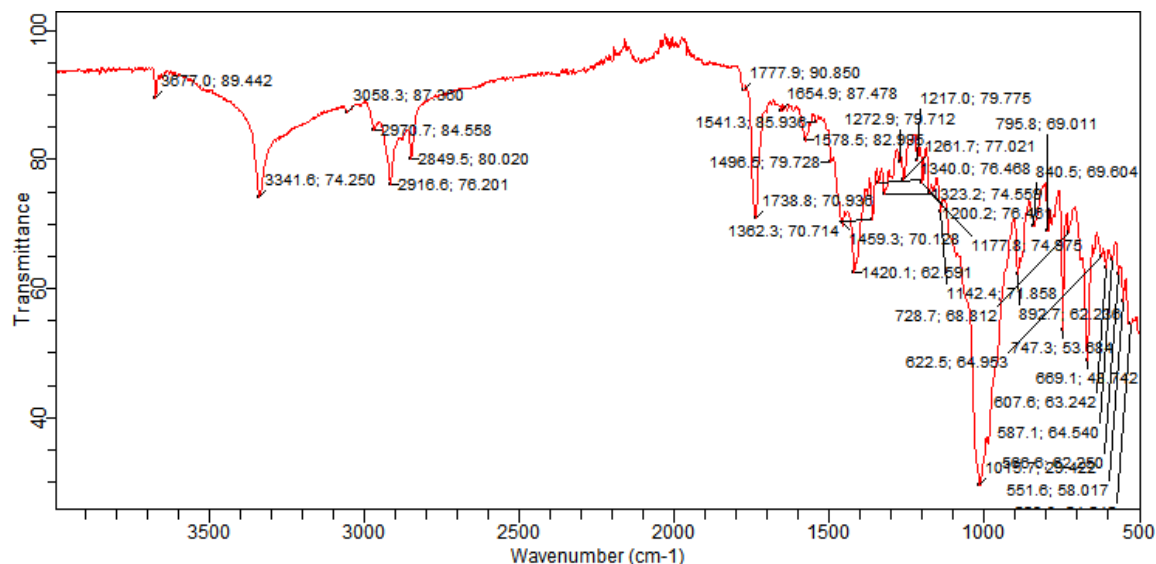


Figure 10 FTIR of Physical Mixture of Optimized Formulation

Table 14 Interaction studies through IR spectroscopy

Stretching	Tapentadol HCl	Formulation
	Peak cm^{-1}	Peak cm^{-1}
C=C	1738.8	1738.8
H-C-H	1362.3	1362.3
C-O	1142.4	1142.4
N-H	3339.7	3341.6
C-H	3056.4	3058.3
C=C	1738.8	1738.8

Conclusion: Based on the FTIR study findings presented above, it was concluded that there were no notable interactions observed between the drug and excipients. Therefore, the drug and other excipients are deemed compatible with each other.

Pre compression Parameters of Trial Batches

Table 15 Result of Pre compression parameters of Trial Batches of Immediate release

Batch	Bulk density (g/ml)(n=3)	Tapped density (g/ml)(n=3)	Carr's index (%) (n=3)	Hausner's ratio (n=3)	Angle of repose (θ°) (n=3)
TF1	0.50 \pm 0.03	0.59 \pm 0.03	12.25 \pm 0.04	1.18 \pm 0.02	32.4 $^\circ$ \pm 1.2
TF2	0.54 \pm 0.04	0.61 \pm 0.02	11.47 \pm 0.02	1.12 \pm 0.04	31.2 $^\circ$ \pm 2.3
TF3	0.45 \pm 0.03	0.52 \pm 0.04	13.46 \pm 0.03	1.15 \pm 0.02	33.1 $^\circ$ \pm 2.5
TF4	0.52 \pm 0.10	0.59 \pm 0.05	11.86 \pm 0.05	1.13 \pm 0.03	34.4 $^\circ$ \pm 3.1
TF5	0.48 \pm 0.05	0.54 \pm 0.03	12.72 \pm 0.05	1.12 \pm 0.04	30.2 $^\circ$ \pm 1.9
TF6	0.56 \pm 0.10	0.63 \pm 0.04	11.11 \pm 0.03	1.12 \pm 0.05	31.3 $^\circ$ \pm 2.4
TF7	0.51 \pm 0.02	0.59 \pm 0.03	13.55 \pm 0.06	1.15 \pm 0.06	34.4 $^\circ$ \pm 2.3
TF8	0.50 \pm 0.04	0.57 \pm 0.02	12.85 \pm 0.03	1.14 \pm 0.04	31.6 $^\circ$ \pm 1.3
TF9	0.54 \pm 0.03	0.62 \pm 0.05	12.90 \pm 0.02	1.14 \pm 0.06	30.3 $^\circ$ \pm 2.3

It can be concluded from the flow property data above that the blended flow is of a good nature and handles compression smoothly.

Table 16 Results of pre compression parameters of Trial Batches of Sustained release

Batch	Bulk density (g/ml)(n=3)	Tapped density (g/ml)(n=3)	Carr's index (%) (n=3)	Hausner's ratio (n=3)	Angle of repose (θ°) (n=3)
TSR1	0.52 ± 0.05	0.60 ± 0.03	13.33 ± 0.05	1.15 ± 0.03	34.2° ± 2.4
TSR2	0.57 ± 0.03	0.66 ± 0.05	13.63 ± 0.03	1.15 ± 0.02	33.5° ± 1.5
TSR3	0.51 ± 0.10	0.57 ± 0.03	10.52 ± 0.03	1.11 ± 0.04	32.1° ± 1.3
TSR4	0.54 ± 0.03	0.61 ± 0.04	11.47 ± 0.02	1.12 ± 0.03	34.5° ± 3.1
TSR5	0.55 ± 0.02	0.62 ± 0.05	11.29 ± 0.05	1.13 ± 0.04	33.1° ± 1.5
TSR6	0.56 ± 0.04	0.64 ± 0.02	12.53 ± 0.06	1.14 ± 0.03	30.2° ± 2.4
TSR7	0.52 ± 0.03	0.59 ± 0.04	11.8 ± 0.03	1.14 ± 0.05	34.2° ± 2.1
TSR8	0.54 ± 0.10	0.61 ± 0.02	11.47 ± 0.05	1.12 ± 0.04	33.7° ± 1.3
TSR9	0.57 ± 0.03	0.65 ± 0.05	12.30 ± 0.02	1.14 ± 0.06	32.2° ± 2.3

Table 17 Results of post compression parameters of Trial Batches of Immediate release

Formulation Code	Weight variation (mg) (n=20)	Thickness (mm) (n=3)	Hardness (kg/cm ²) (n=3)	Friability %	Drug content % (n=3)	Disintegration time
TIR1	250.13±0.05	3.74±0.01	4.53±0.17	0.62±0.04	98.72±0.02	126 sec
TIR2	250.25±0.04	3.93±0.05	5.25±0.12	0.78±0.07	96.96±0.01	109 sec
TIR3	248.88±0.26	3.49±0.03	5.0±0.13	0.57±0.03	97.44±0.05	90 sec
TIR4	250.25±0.35	3.63±0.03	5.48±0.16	0.68±0.07	95.68±0.04	120 sec
TIR5	250.28±0.04	3.57±0.04	4.85±0.13	0.59±0.06	97.61±0.02	96 sec
TIR6	250.87±0.34	4.35±0.07	5.50±0.15	0.61±0.09	98.80±0.03	83 sec
TIR7	249.99±0.23	3.23±0.09	4.94±0.17	0.59±0.06	96.91±0.03	92 sec
TIR8	251.65±0.26	3.14±0.06	5.33±0.11	0.69±0.05	93.73±0.03	74 sec
TIR9	250.22±0.16	3.56±0.03	5.30±0.13	0.54±0.02	98.12±0.03	40 sec

Table 18 Results of post compression parameters of Trial Batches of Sustained release

Formulation Code	Weight variation (mg) (n=20)	Thickness (mm) (n=3)	Hardness (kg/cm ²) (n=3)	Friability %	Drug content % (n=3)
TSR1	600.80±0.02	5.50±0.03	5.57±0.12	0.48±0.05	97.47±0.02
TSR2	600.25±0.04	5.59±0.01	5.30±0.15	0.60±0.02	96.45±0.01
TSR3	600.47±0.22	5.63±0.04	6.00±0.13	0.57±0.07	97.58±0.05
TSR4	600.30±0.5	6.22±0.03	5.49±0.12	0.59±0.03	99.28±0.04
TSR5	600.50±0.04	5.57±0.04	5.89±0.15	0.63±0.06	98.82±0.02
TSR6	600.72±0.2	5.70±0.05	5.50±0.15	0.54±0.04	97.35±0.03
TSR7	600.99±0.23	5.53±0.07	6.2±0.13	0.60±0.06	96.91±0.03

TSR8	600.65±0.26	5.50±0.02	5.30±0.11	0.63±0.02	97.53±0.03
TSR9	600.22±0.16	5.56±0.03	5.00±0.13	0.59±0.05	98.42±0.03

In Vitro Drug Release Study

Preliminary Trials

Table 19 Drug release of Trial Batches of Immediate release

Time(min)	F1	F2	F3	F4	F5	F6	F7	F8	F9
0	0±0.0	0±0.0	0±0.0	0±0.0	0±0.0	0±0.0	0±0.0	0±0.0	0±0.0
5	15.1± 4.5	20.4± 3.1	23.8± 4.2	20.9± 3.0	28.4± 2.8	31.2± 3.6	25.6± 2.8	32.4± 1.9	39.5 ±3.6
10	22.0 ±2.9	37.9± 2.8	41.2± 3.3	27.5± 2.8	38.3± 2.4	44.8± 2.8	32.7± 2.4	47.5± 1.6	51.6 ±2.8
15	37.4 ±3.4	45.5± 2.6	47.8± 2.5	41.1± 2.1	50.7± 2.2	57.3± 2.4	46.2± 2.3	59.6± 1.3	67.3 ±2.4
20	49.3 ±2.7	59.6± 2.4	61.4± 2.3	53.5± 1.9	65.9± 1.9	69.6± 2.1	59.9± 2.1	71.4± 1.4	83.6 ±2.3
25	62.2 ±2.3	68.3± 2.3	74.3± 2.0	64.3± 1.4	76.6± 1.5	79.1± 2.0	70.4± 2.6	83.5± 1.1	90.4 ±1.8
30	70.1 ± 2.5	80.9 ±2.1	88.9± 1.6	76.4± 1.2	85.4± 1.2	91.7± 1.5	83.7± 1.5	90.3± 1.0	98.8 ±1.4

Table 20 Drug release of Trial Batches of Sustained release

Time(hour)	TSR1	TSR2	TSR3	TSR4	TSR5	TSR6	TSR7	TSR8	TSR9
1	37.5± 4.4	32.1± 2.5	29.5± 4.2	35.4± 4.3	30.1 ±3.8	24.2± 4.2	30.5± 4.0	26.7± 3.6	20.6± 3.0
2	40.6 ±3.6	39.2± 3.6	36.8± 3.6	39.5± 4.1	36.3± 3.4	31.7± 4.1	42.1± 4.2	33.4± 3.5	25.3± 2.6
3	47.1± 2.1	44.9± 1.5	46.2± 3.2	48.2± 3.7	45.4± 3.1	40.7± 3.7	49.4± 3.7	39.7± 3.1	31.5± 2.4
4	58.4± 1.2	56.6± 1.7	53.0± 2.9	56.9± 3.5	51.7± 2.7	45.1± 3.2	53.7± 3.4	44.1± 2.8	38.4± 2.1
5	63.6± 1.7	60.7± 1.2	59.4± 2.7	60.2± 2.6	59.6± 2.4	52.8± 3.4	58.3± 2.3	51.6± 2.6	46.8± 2.6
6	72.5± 2.0	68.6± 1.5	62.7± 1.8	65.3± 2.3	61.7± 2.1	59.3± 2.3	63.6± 2.2	58.3± 2.5	50.1± 2.4
7	86.2± 1.9	82.6± 2.1	71.1± 2.4	73.2± 3.2	69.8± 2.5	68.1± 2.4	70.4± 2.4	63.9± 2.4	57.5± 2.4
8	91.0± 1.5	89.3± 1.6	74.2± 1.5	81.5± 2.9	77.4± 1.6	72.5± 2.6	74.5± 2.5	69.4± 2.3	63.6± 2.9
9	97.7± 2.2	93.0± 1.5	80.6± 1.7	91.6± 2.1	82.2± 1.4	79.4± 2.4	78.4± 2.8	73.2± 1.8	67.3± 1.8
10	99.2± 2.1	95.5± 1.7	84.5± 1.4	96.4± 1.4	87.9± 1.3	83.8± 2.1	82.8± 1.4	79.7± 1.6	73.4± 1.2
11	-	98.6± 1.1	87.4± 2.4	99.5± 1.1	92.6± 1.3	93.3± 1.5	87.9± 1.3	82.4± 1.3	77.3± 1.4
12	-	-	91.1± 2.6	-	98.4± 1.2	95.6± 1.2	93.5± 1.1	87.1± 1.1	84.8± 1.2

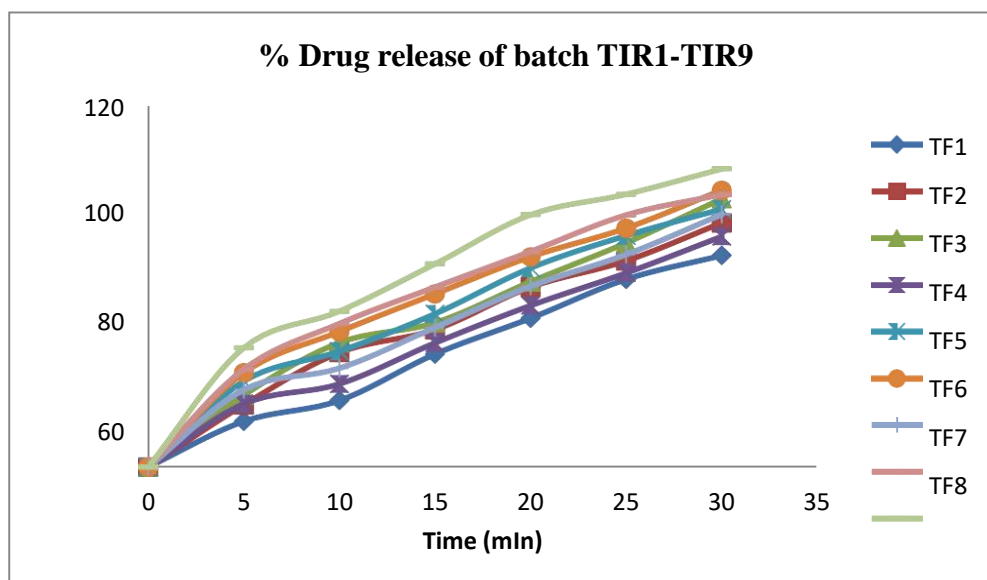


Figure 11 Drug release of Batch T1-T9of Trial Batches of immediate release

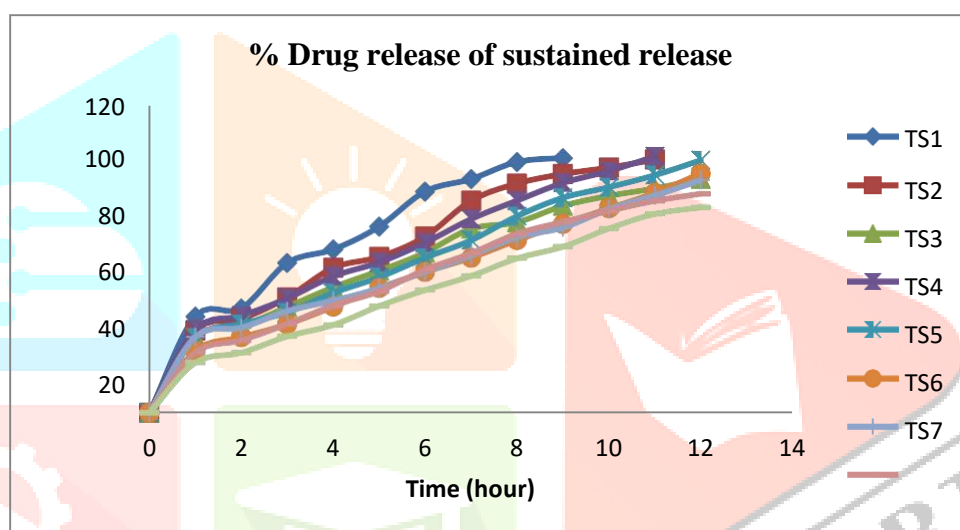


Figure 12 Drug release of Batch T1-T9 of Trial Batches of sustained release

Evaluation of factorial batches

Powder blend of factorial batches F1-F9 checked for pre-compression parameters. Observed results are mentioned in following table 6.9. From the below table it concluded that the all batches have a good flow properties.

Table 21 Results of Pre compression parameters of factorial batches of immediate release

Formulation Code	Bulk density (g/ml) (n=3)	Tapped density (g/ml) (n=3)	% Carr's index (n=3)	Hausner's ratio (n=3)	Angle of repose
FIR1	0.50 ± 0.02	0.59 ± 0.02	15.25 ± 0.02	1.18 ± 0.02	32.4±0.04
FIR2	0.45 ± 0.04	0.52 ± 0.05	13.46 ± 0.06	1.15 ± 0.07	34.2±0.03
FIR3	0.52 ± 0.05	0.59 ± 0.03	11.86 ± 0.02	1.12 ± 0.08	30.1±.002
FIR4	0.54 ± 0.02	0.62 ± 0.03	12.90 ± 0.04	1.14 ± 0.05	32.4±0.03
FIR5	0.55 ± 0.03	0.62 ± 0.05	11.29 ± 0.05	1.12 ± 0.06	33.6±0.02

FIR6	0.56 ± 0.05	0.63 ± 0.04	11.11 ± 0.08	1.12 ± 0.04	31.3±0.02
FIR7	0.52 ± 0.04	0.59 ± 0.06	11.86 ± 0.07	1.13± 0.08	31.7±0.03
FIR8	0.56 ± 0.06	0.63 ± 0.04	11.11 ± 0.05	1.12± 0.02	30.0±0.04
FIR9	0.53 ± 0.05	0.61 ± 0.04	13.11 ± 0.04	1.15± 0.06	31.2±0.01

Table 22 Results of Pre compression parameters of factorial batches of sustained release

Formulation Code	Bulk density (g/ml) (n=3)	Tapped density (g/ml) (n=3)	% Carr's index (n=3)	Hausner's ratio (n=3)	Angle of repose
FSR1	0.52 ± 0.03	0.59 ± 0.03	11.86 ± 0.04	1.13 ± 0.02	32.2±0.02
FSR2	0.54 ± 0.02	0.61 ± 0.05	11.47 ± 0.02	1.12 ± 0.07	32.5±0.02
FSR3	0.57 ± 0.04	0.65 ± 0.02	12.30 ± 0.05	1.14 ± 0.08	31.1±0.04
FSR4	0.54 ± 0.05	0.61 ± 0.04	11.47 ± 0.04	1.12 ± 0.05	32.3±0.03
FSR5	0.53 ± 0.02	0.62 ± 0.05	14.51 ± 0.03	1.16 ± 0.06	30.3±0.02
FSR6	0.56 ± 0.03	0.64 ± 0.03	12.5 ± 0.06	1.14 ± 0.04	32.1±0.04
FSR7	0.51 ± 0.04	0.59 ± 0.05	13.55 ± 0.05	1.15± 0.08	31.4±0.05
FSR8	0.55 ± 0.02	0.63 ± 0.06	12.69 ± 0.07	1.14± 0.02	31.2±0.03
FSR9	0.52 ± 0.04	0.59 ± 0.03	11.86 ± 0.03	1.13± 0.06	30.7±0.02

Table 23 Results of Post compression parameters of factorial batches of immediate release

Formulation Code	Weight variation (mg) (n=20)	Thick-ness (mm) (n=3)	Hard-ness (kg/cm²) (n=3)	Friability %	Drug content % (n=3)	Disintegration Time (Sec)
FIR1	249.21 ±0.19	3.72±0.05	5.60±0.10	0.66±0.01	97.25 ±0.05	120sec
FIR2	251.13 ±0.28	3.36±0.09	5.29±0.15	0.62±0.02	97.10 ±0.04	109 sec
FIR3	252.15 ±0.36	3.45±0.08	5.30±0.09	0.59±0.06	98.45 ±0.03	103 sec
FIR4	249.36 ±0.39	4.15±0.05	4.78±0.13	0.63±0.02	98.14 ±0.04	92 sec
FIR5	250.54 ±0.45	3.49±0.07	5.10±0.19	0.58±0.08	97.65 ±0.07	83 sec
FIR6	251.12 ±0.29	4.30±0.08	4.85±0.12	0.62±0.03	99.42 ±0.02	70 sec
FIR7	249.99 ±0.36	3.15±0.03	5.15±0.11	0.61±0.01	98.41 ±0.04	58 sec
FIR8	250.46 ±0.42	3.45±0.05	5.57±0.13	0.56±0.03	98.36 ±0.05	36 sec

FIR9	251.42 ±0.28	3.89±0.0 6	5.50±0.1 8	0.58±0.05	96.25 ±0.06	48 sec
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Table 24 Results of post compression parameters of factorial batches of sustained release

Formulation code	Weight variation (mg) (n = 3)	Thickness (mm) (n = 3)	Hardness (kg/cm ²) (n = 3)	Friability % (n = 3)	Drug Content % (n = 3)
FSR 1	599.25 ±0.13	5.23±0.03	5.20±0.10	0.64±0.0 3	97.38 ±0.02
FSR 2	600.15 ±0.26	5.39±0.04	5.34±0.15	0.62±0.0 2	98.47 ±0.04
FSR 3	601.12 ±0.39	5.85±0.05	5.82±0.09	0.66 ±0.04	97.57 ±0.03
FSR 4	599.39 ±0.26	5.65±0.02	6.32±0.13	0.55±0.0 6	99.14 ±0.01
FSR 5	600.54 ±0.36	5.15±0.04	5.32±0.19	0.58±0.0 3	98.74 ±0.03
FSR 6	600.11 ±0.20	5.53±0.07	5.85±0.12	0.62±0.0 5	98.34 ±0.02
FSR 7	601.76 ±0.25	5.36±0.03	5.52±0.11	0.59±0.0 2	98.12 ±0.03
FSR 8	599.59 ±0.58	6.25±0.05	5.57±0.13	0.57±0.0 4	97.16 ±0.02
FSR 9	601.42 ±0.28	5.37±0.06	5.50±0.18	0.64±0.0 6	98.42 ±0.02

Drug release

Drug release of factorial batches was performed to check the impact of the amount of polymer and efferent agent. Based on results it found that the amount of polymer change the release profile of the tablets. The actual impact was checked by using factorial design. The comparative plot was shown in below figure.

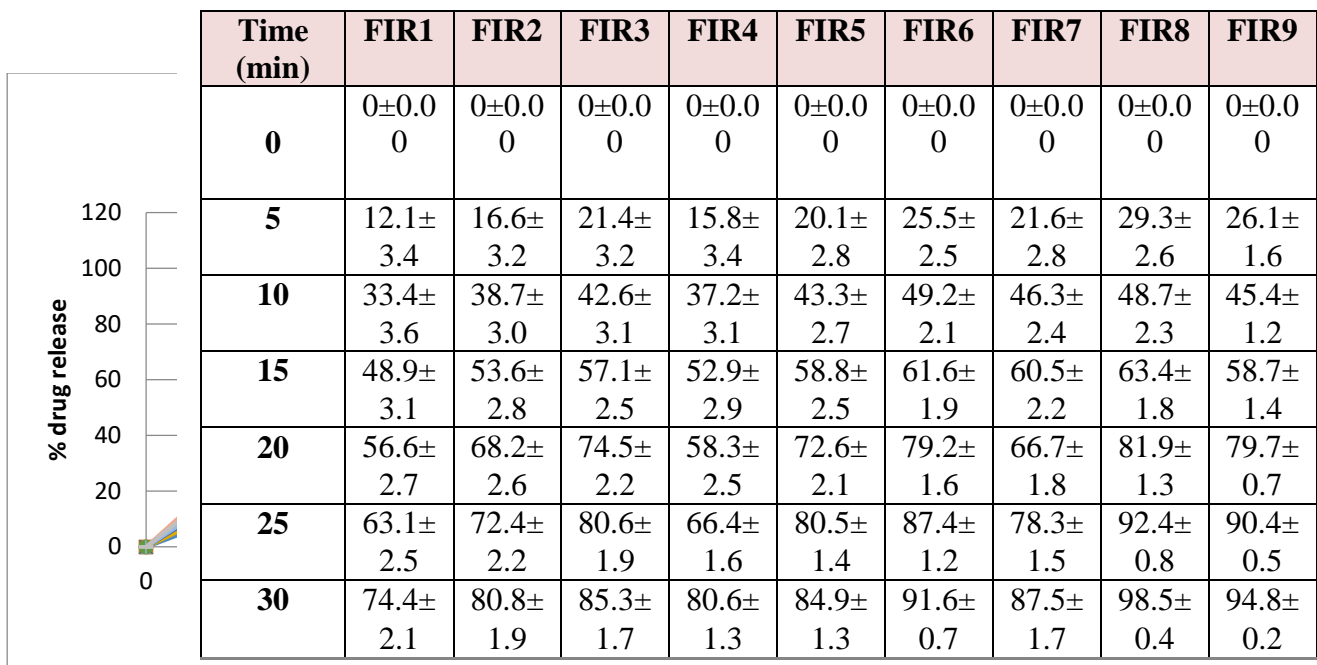
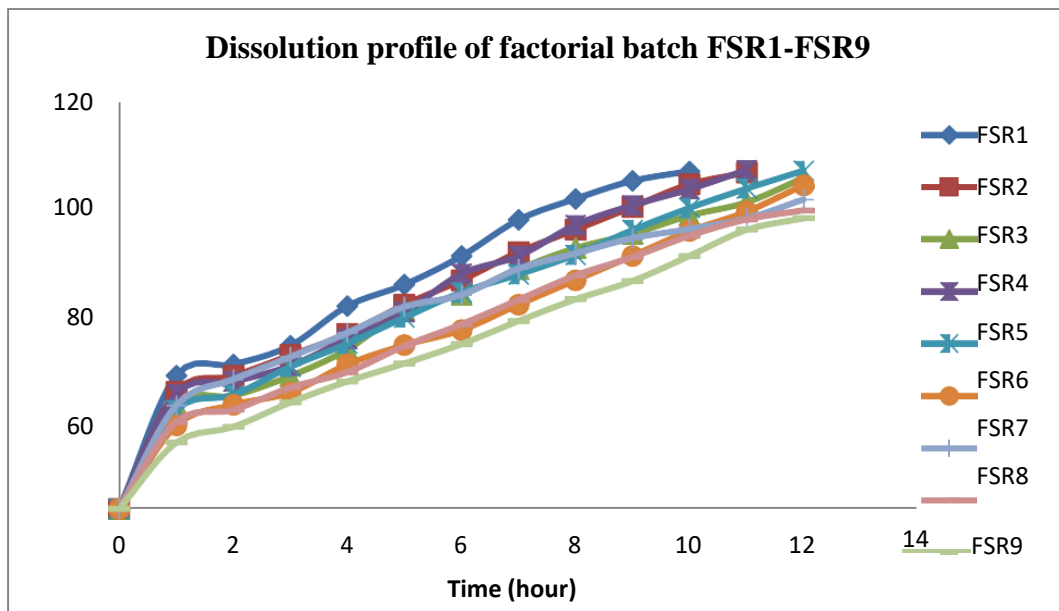


Figure 13 Drug release profile of TIR1-TIR9

Table 25 drug release profile of sustained release layer

Time (hour)	FSR1	FSR2	FSR3	FSR4	FSR5	FSR6	FSR7	FSR8	FSR9
1	39.3±4.6	34.5±4.3	30.1±3.8	33.8±4.8	29.1±4.3	24.6±4.6	30.5±4.1	25.7±3.9	19.6±4.8
2	42.6±4.3	39.2±4.1	33.4±3.5	37.5±4.4	33.6±4.1	30.7±4.0	38.2±3.9	29.2±3.6	24.2±4.4
3	48.1±4.1	45.3±3.8	39.2±3.1	42.2±4.1	41.9±3.8	34.3±3.8	44.8±3.7	35.8±3.4	31.4±4.1
4	59.8±3.9	51.6±3.6	47.0±2.9	50.1±3.8	48.7±3.7	42.6±3.6	51.9±3.2	40.3±3.1	37.6±3.8
5	66.1±3.6	60.2±3.0	58.6±2.8	57.9±3.6	56.4±3.4	48.3±3.5	59.6±2.8	48.0±2.9	42.9±3.5
6	74.5±3.1	67.4±2.8	63.2±2.5	69.3±3.2	63.8±3.2	52.7±3.1	63.1±2.7	54.4±2.6	48.6±3.2
7	85.2±3.0	75.7±2.6	70.7±2.1	74.5±2.5	69.1±2.9	60.2±2.8	70.8±2.4	61.6±2.4	55.4±3.1
8	91.4±2.7	82.3±2.5	76.9±1.8	83.7±2.5	74.9±2.5	67.4±2.5	75.3±2.1	68.8±2.7	61.8±2.9
9	96.7±2.1	89.0±1.9	81.1±1.6	89.5±2.4	82.2±1.6	74.6±2.0	79.8±1.7	74.2±2.2	67.2±2.6
10	99.5±0.2	95.7±1.5	86.5±1.5	94.2±1.3	88.7±1.4	81.9±1.7	82.5±1.5	80.5±2.5	74.6±2.4
11	-	99.1±0.3	90.4±1.5	99.9±0.03	94.4±0.8	87.6±1.4	85.6±1.4	85.3±3.5	82.3±2.7
12	-	-	95.2±1.3	-	97.2±0.5	94.4±1.1	91.2±1.7	88.0±3.0	85.7±2.8



Drug Release Kinetic Study

In vitro drug release study data was fitted in kinetic models and results obtained were shown in below table 6.13. Formulation was best fitted with **Korsmeyer Peppas** model and mechanism of drug release was found to be Non-Fickian type of diffusion.

Table 26 Drug Release Kinetic Study of factorial batches FIR1-FIR9

FORMULATIONS	ZERO ORDER	FIRST ORDER	HIGUCHI MODEL	KORS PEPAS
FIR1	0.952	0.803	0.987	0.954
FIR2	0.944	0.823	0.985	0.967
FIR3	0.944	0.850	0.982	0.978
FIR4	0.957	0.831	0.983	0.965
FIR5	0.939	0.827	0.983	0.970
FIR6	0.947	0.855	0.984	0.979
FIR7	0.951	0.832	0.985	0.966
FIR8	0.973	0.909	0.993	0.995
FIR9	0.968	0.904	0.986	0.991

Table 27 Drug Release Kinetic Study of factorial batches FSR1-FSR9

FORMULATIONS	ZERO ORDER	FIRST ORDER	HIGUCHI MODEL	KORS PEPAS
FSR1	0.992	0.988	0.977	0.977
FSR2	0.996	0.997	0.979	0.978
FSR3	0.989	0.979	0.982	0.981
FSR4	0.987	0.991	0.968	0.966
FSR5	0.996	0.977	0.996	0.997
FSR6	0.991	0.984	0.980	0.976
FSR7	0.993	0.981	0.991	0.992

FSR8	0.996	0.993	0.981	0.985
FSR9	0.866	0.632	0.911	0.776

Analysis of factorial design for immediate release

The obtained results were compiled for analysis using factorial design. The factors and responses tabulated in software than analysis was done using below table.

Table 28 Factorial design analysis table of immediate release

Batch	Lactose (mg)	Crosspovidone (mg)	Disintegration time (sec)	% drug release
FIR1	110	7.5	120	74.4
FIR2	110	12.5	109	80.8
FIR3	110	17.5	103	85.3
FIR4	115	7.5	92	80.6
FIR5	115	12.5	83	84.9
FIR6	115	17.5	70	91.6
FIR7	120	7.5	58	87.5
FIR8	120	12.5	33	98.5
FIR9	120	17.5	48	94.8

ANOVA for Quadratic model

Response 1: Disintegration time

Table 29 ANOVA of response 1 for immediate release

Source	Sum of Squares	df	Mean Square	F-value	p-value	
Model	6511.36	5	1302.27	25.12	0.0118	Significant
A-lactose	6016.67	1	6016.67	116.06	0.0017	
B-crosspovidone	400.17	1	400.17	7.72	0.0691	
AB	12.25	1	12.25	0.2363	0.6602	
A ²	14.22	1	14.22	0.2743	0.6367	
B ²	68.06	1	68.06	1.31	0.3350	
Residual	155.53	3	51.84			
Cor Total	6666.89	8				

Factor coding is **coded**.

Sum of squares is **Type III - Partial**

The **Model F-value** of 25.12 implies the model is significant. There is only a 1.18% chance that an F-value this large could occur due to noise.

P-values Model terms are considered significant when P-values are less than 0.0500. A is a significant model term in this instance. The model features are not significant if the value is

bigger than 0.1000. Model reduction could make your model better if it has a large number of unimportant model terms (apart from those needed to maintain hierarchy).

Coefficients in Terms of Coded Factors

Table 30 Coefficient factor of response 1 for immediate release layer

Factor	Coefficient Estimate	df	Standard Error	95% CI Low	95% CI High	VIF
Intercept	77.78	1	5.37	60.70	94.86	
A-lactose	-31.67	1	2.94	-41.02	-22.31	1.0000
B-crosspovidone	-8.17	1	2.94	-17.52	1.19	1.0000
AB	1.75	1	3.60	-9.71	13.21	1.0000
A ²	-2.67	1	5.09	-18.87	13.54	1.0000
B ²	5.83	1	5.09	-10.37	22.04	1.0000

Polynomial Equation :- $Y_1 = 77.78 - 31.67X_1 - 8.17X_2 + 1.75X_{12} - 2.67X_1^2 + 5.83X_2^2$

When all other factors are maintained constant, the coefficient estimate shows the expected change as a result for each unit change in parameter value. The total average response of all the runs is the intercept in an orthogonal design. Based on the factor parameters, the coefficients are adjustments around that average. VIFs are 1 when the factors are orthogonal; VIFs larger than 1 denote multi-collinearity; the higher the VIF, the more severe the factor correlation. VIFs of fewer than 10 are generally acceptable.

Design-Expert® Software
Factor Coding: Actual

Disintegration time (sec)

● Design Points
36 120

X1 = A: lactose
X2 = B: crosspovidone

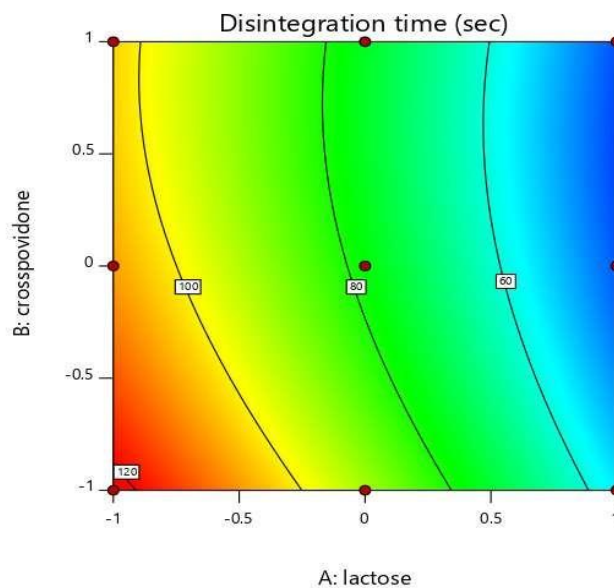


Figure 15 Counter plot of disintegration time

fi

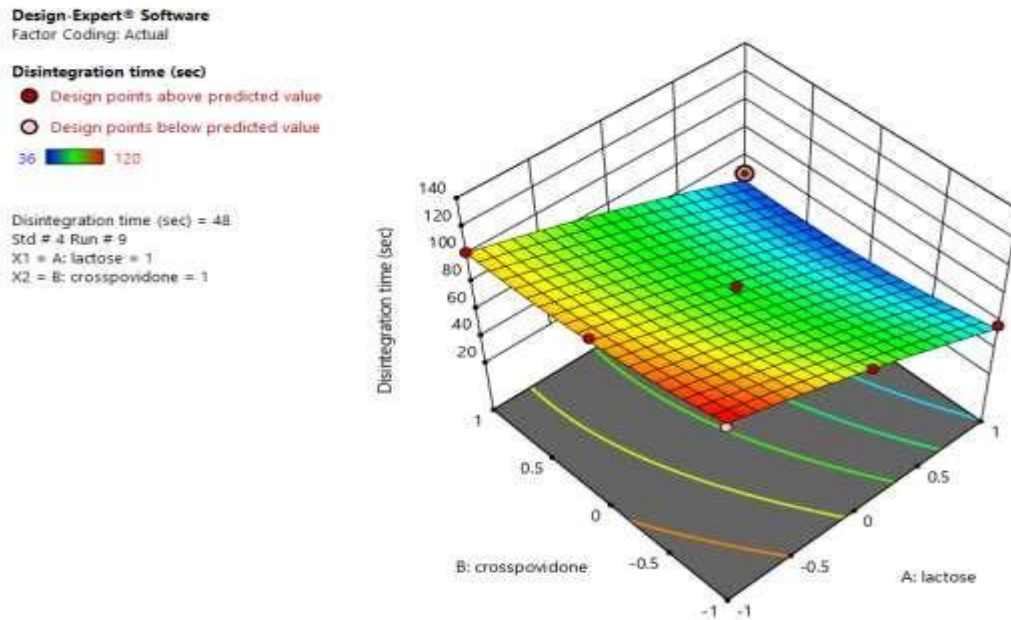


Figure 16 Surface Plot of Disintegration Time

ANOVA for Quadratic model

Response 2: %drug release

Table 31 ANOVA data of response 2 for immediate release layer

Source	Sum of Squares	df	Mean Square	F-value	p-value	
Model	430.03	5	86.01	9.36	0.0475	Significant
A-lactose	270.68	1	270.68	29.45	0.0123	
B-crosspovidone	142.11	1	142.11	15.46	0.0293	
AB	3.24	1	3.24	0.3525	0.5945	
A ²	2.80	1	2.80	0.3047	0.6194	
B ²	11.20	1	11.20	1.22	0.3502	
Residual	27.58	3	9.19			
Cor Total	457.61	8				

Factor coding is coded.

Sum of squares is **Type III – Partial** The **Model F-value** of 9.36 implies the model is significant. There is only a 4.75% chance that an F-value this large could occur due to noise.

P-values less than 0.0500 indicate model terms are significant. In this case A, B are significant model terms. Values greater than 0.1000 indicate the model terms are not significant. If there are many insignificant model terms (not counting those required to support hierarchy), model reduction may improve your model.

Coefficients in Terms of Coded Factors

Table 32 Coefficient data of response 2 for immediate release layer

Factor	Coefficient Estimate	df	Standard Error	95% CI Low	95% CI High	VIF
Intercept	87.28	1	2.26	80.09	94.47	
A-lactose	6.72	1	1.24	2.78	10.66	1.0000
B-crosspovidone	4.87	1	1.24	0.9275	8.81	1.0000

AB	-0.9000	1	1.52	-5.72	3.92	1.0000
A ²	1.18	1	2.14	-5.64	8.01	1.0000
B ²	-2.37	1	2.14	-9.19	4.46	1.0000

Polynomial Equation

$$Y_2 = 87.82 + 6.72X_1 + 4.87X_2 - 0.9000X_{12} + 1.18X_1^2 - 2.37X_2^2$$

The coefficient estimate, assuming that all other factors remain constant, shows the anticipated change in response for each unit change in factor value. In an orthogonal design, the intercept represents the mean response of all the runs combined. The factor settings' adjustments around that average are represented by the coefficients. VIFs of one indicate orthogonality; those of larger than one suggest multi-collinearity; the higher the VIF, the more severe the factor correlation. VIFs under 10 are generally considered tolerable.

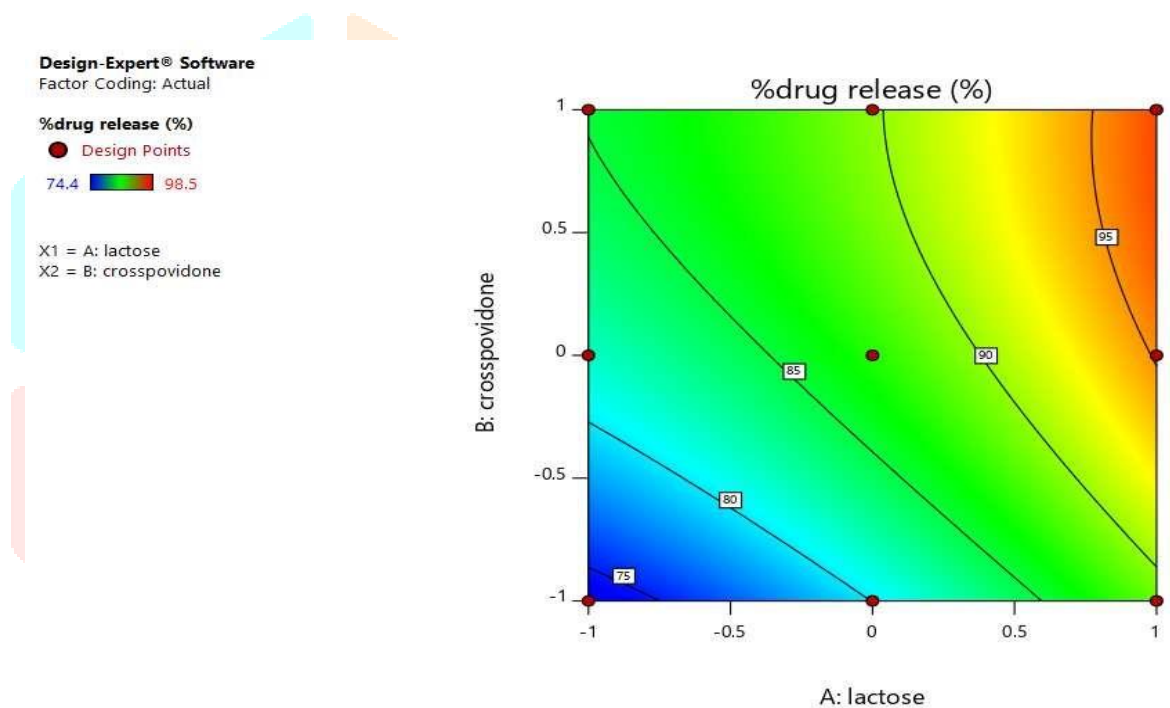


Figure 17 Counter plot of % drug release

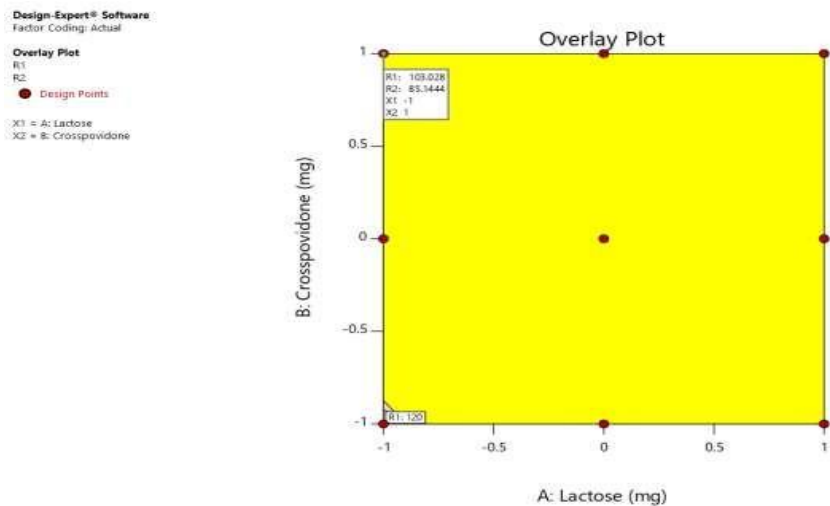


Figure 20 Check point batch for immediate releas

Analysis of factorial design for sustained release

Design-Expert® Software
Factor Coding: Actual

%drug release (%)

- Design points above predicted value
- Design points below predicted value

74.4 98.5

X1 = A: lactose
X2 = B: crosspovidone

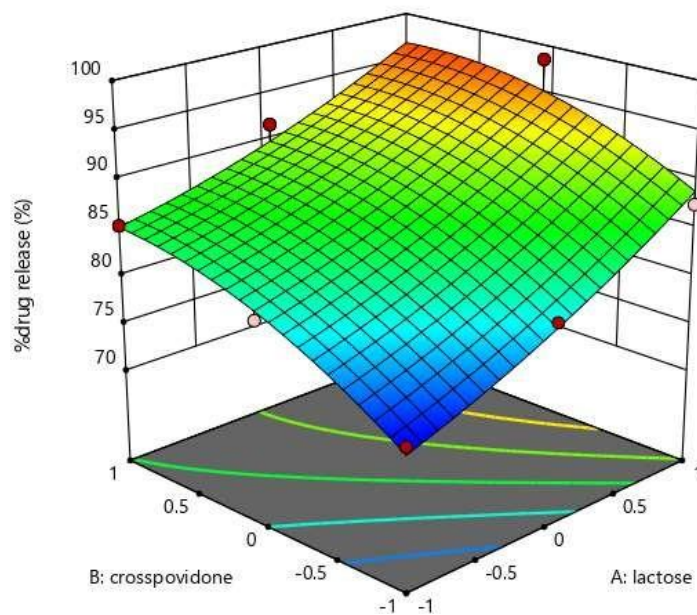


Figure 18 surface plot of % drug release

Utilizing data fitting in design expert software, the design is analyzed.

Table 33 Factorial design analysis table of sustained release

Batch	PVP K 30 (%)	Kolloidon SR (%)	Hardness (kg/cm ²)	% drug release At 1 hour
FSR1	2	8	5.5	39.3
FSR2	2	10	5.7	34.5
FSR3	2	12	5.8	30.7
FSR4	2.5	8	5.5	33.8
FSR5	2.5	10	5.9	29.1
FSR6	2.5	12	6.0	24.6
FSR7	3	8	5.9	30.5
FSR8	3	10	6.0	25.7
FSR9	3	12	6.3	19.6

ANOVA for Quadratic model

Response 1: Hardness

Table 34 ANOVA model of response 1 for sustained release

Source	Sum of Squares	df	Mean Square	F-value	p-value	
Model	2.07	5	0.4132	68.70	0.0027	significant
A-PVP K 30	1.82	1	1.82	301.75	0.0004	
B-Kolloidon SR	0.0241	1	0.0241	4.00	0.1393	
AB	0.0484	1	0.0484	8.05	0.0658	
A ²	0.0601	1	0.0601	9.99	0.0508	
B ²	0.1184	1	0.1184	19.69	0.0213	
Residual	0.0180	3	0.0060			
Cor Total	2.08	8				

Factor coding is **coded**.

Sum of squares is **Type III - Partial**

The **Model F-value** of 68.70 implies the model is significant. There is only a 0.27% chance that an F-value this large could occur due to noise.

P-values less than 0.0500 indicate model terms are significant. In this case A, B² are significant model terms. Values greater than 0.1000 indicate the model terms are not significant. If there are many insignificant model terms (not counting those required to support hierarchy), model reduction may improve your model.

Fit Statistics

Std. Dev.	0.0776	R²	0.9913
Mean	5.06	Adjusted R²	0.9769
C.V. %	1.53	Predicted R²	0.9018
		Adeq Precision	23.9511

The **Predicted R²** of 0.9018 is in reasonable agreement with the **Adjusted R²** of 0.9769; i.e. the difference is less than 0.2.

Adeq Precision calculates the ratio of signal to noise. Ideally, the ratio should be higher than 4. With a ratio of 23.951, you have a sufficient signal. The design space can be navigated using this concept..

Coefficients in Terms of Coded Factors

Table 35 Coefficient data of response 1 for sustained release

Factor	Coefficient Estimate	Df	Standard Error	95% Low	CI 95% High	CIVIF
Intercept	5.34	1	0.0578	5.16	5.53	
A-PVP K 30	0.5500	1	0.0317	0.4492	0.6508	1.0000
B-Kolloidon SR	0.0633	1	0.0317	-0.0374	0.1641	1.0000
AB	-0.1100	1	0.0388	-0.2334	0.0134	1.0000
A ²	-0.1733	1	0.0548	-0.3479	0.0012	1.0000
B ²	-0.2433	1	0.0548	-0.4179	-0.0688	1.0000

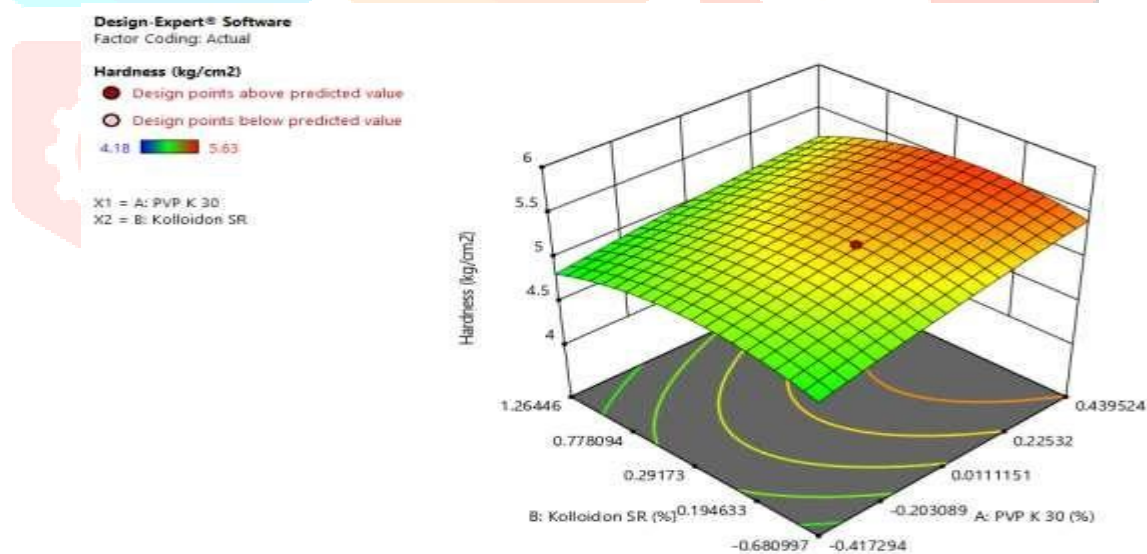


Figure 21 Surface plot of Hardness

Polynomial Equation

$$Y1 = 5.34 + 0.550X1 + 0.0633X2 - 0.1100X12 - 0.1733X1^2 - 0.2433X2^2$$

When all other factors are maintained constant, the coefficient estimate shows the expected change in response for each unit change in factor value. The total average response of all the runs is the intercept in an orthogonal design. Based on the factor parameters, the coefficients are adjustments around that average. VIFs are 1 when the factors are orthogonal; VIFs larger than 1 denote multi-collinearity; the higher

the VIF, the more severe the factor correlation. VIFs of fewer than 10 are generally acceptable.

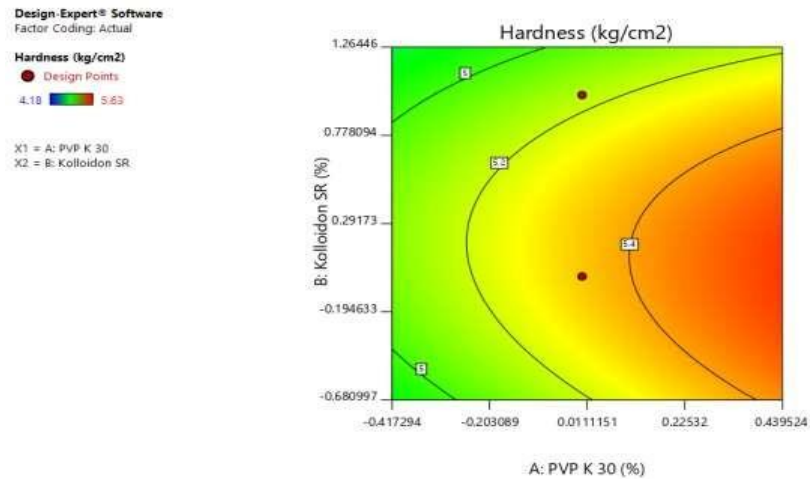


Figure 20-1 Counter plot of Hardness

ANOVA for Quadratic model

Response 2: % drug release

Table 36 ANOVA model of response 2 for sustained release

Source	Sum of Squares	df	Mean Square	F-value	p-value	
Model	211.79	5	42.36	67.12	0.0028	Significant
A-PVP K 30	139.20	1	139.20	220.57	0.0007	
B-Kolloidon SR	39.01	1	39.01	61.82	0.0043	
AB	0.3600	1	0.3600	0.5704	0.5050	
A ²	32.81	1	32.81	51.98	0.0055	
B ²	0.4050	1	0.4050	0.6417	0.4817	
Residual	1.89	3	0.6311			
Cor Total	213.68	8				

Factor coding is **Coded**.

Sum of squares is **Type III - Partial**

The **Model F-value** of 67.12 implies the model is significant. There is only a 0.28% chance that an F-value this large could occur due to noise.

P-values less than 0.0500 indicate model terms are significant. In this case A, B, A² are significant model terms. Values greater than 0.1000 indicate the model terms are not significant. If there are many insignificant model terms (not counting those required to support hierarchy), model reduction may improve your model.

Fit Statistics

Std. Dev.	0.7944	R²	0.9911
Mean	94.47	Adjusted R²	0.9764
C.V. %	0.8410	Predicted R²	0.8955
		Adeq Precision	22.7140

The **Predicted R²** of 0.8955 is in reasonable agreement with the **Adjusted R²** of 0.9764; i.e. the difference is less than 0.2.

Adeq Precision measures the signal to noise ratio. A ratio greater than 4 is desirable. Your ratio of 22.714 indicates an adequate signal. This model can be used to navigate the design space.

Coefficients in Terms of Coded Factors

Table 37 Coefficient data of response 2 for sustained release

Factor	Coefficient Estimate	Df	Standard Error	95% CI Low	95% CI High	VIF
Intercept	97.47	1	0.5921	95.58	99.35	
A-PVP K 30	-4.82	1	0.3243	-5.85	-3.78	1.0000
B-Kolloidon SR	-2.55	1	0.3243	-3.58	-1.52	1.0000
AB	-0.3000	1	0.3972	-1.56	0.9641	1.0000
A ²	-4.05	1	0.5617	-5.84	-2.26	1.0000
B ²	-0.4500	1	0.5617	-2.24	1.34	1.0000

Polynomial Equation

$$Y_2 = 97.47 - 4.82X_1 - 2.55X_2 - 0.3000X_1X_2 - 4.05X_1^2 - 0.4500X_2^2$$

The estimated coefficient of determination shows the anticipated shift in response for each unit change in factor value, assuming that all other factors remain constant. The average reaction over all runs in an orthogonal design is called the intercept. The factor settings determine how the coefficients are adjusted around that average. Orthogonal factors have VIFs of 1, while multi-collinearity is indicated by VIFs more than 1. The more severe the factor correlation, the higher the VIF. Tolerable VIFs are generally less than 10.

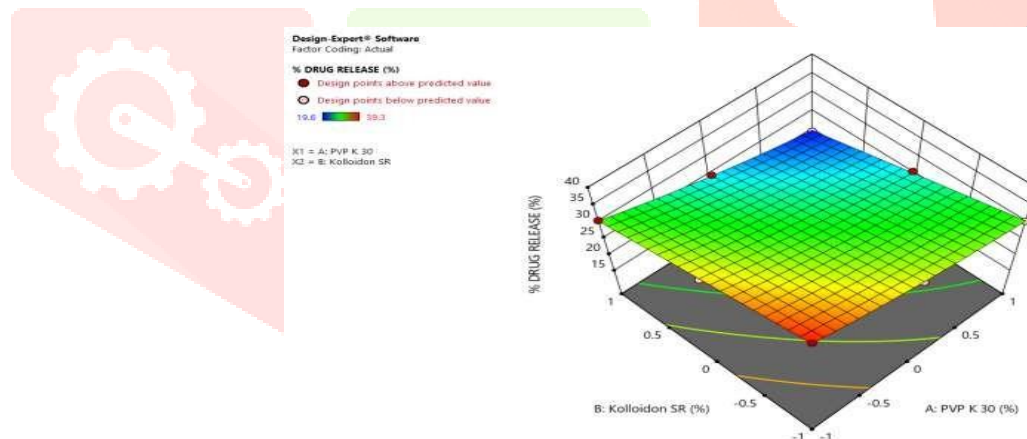


Figure 23 Surface Plot of drug release

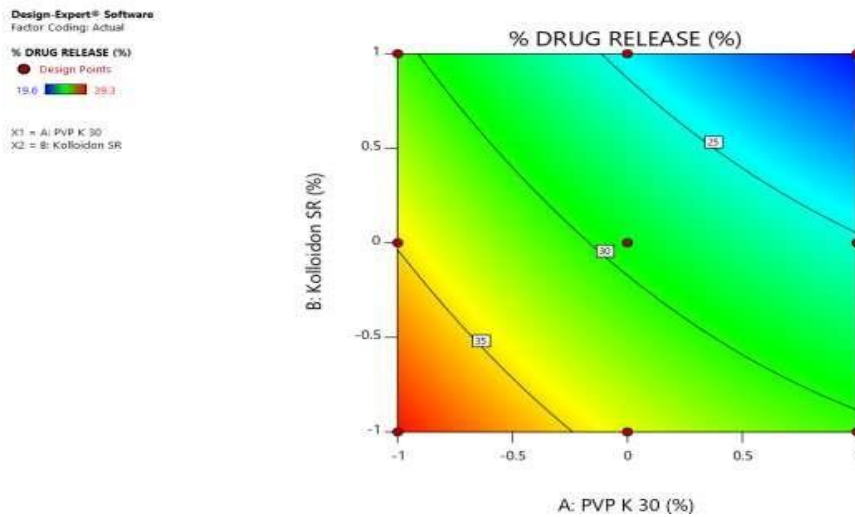


Figure 24 Counter plot of drug release

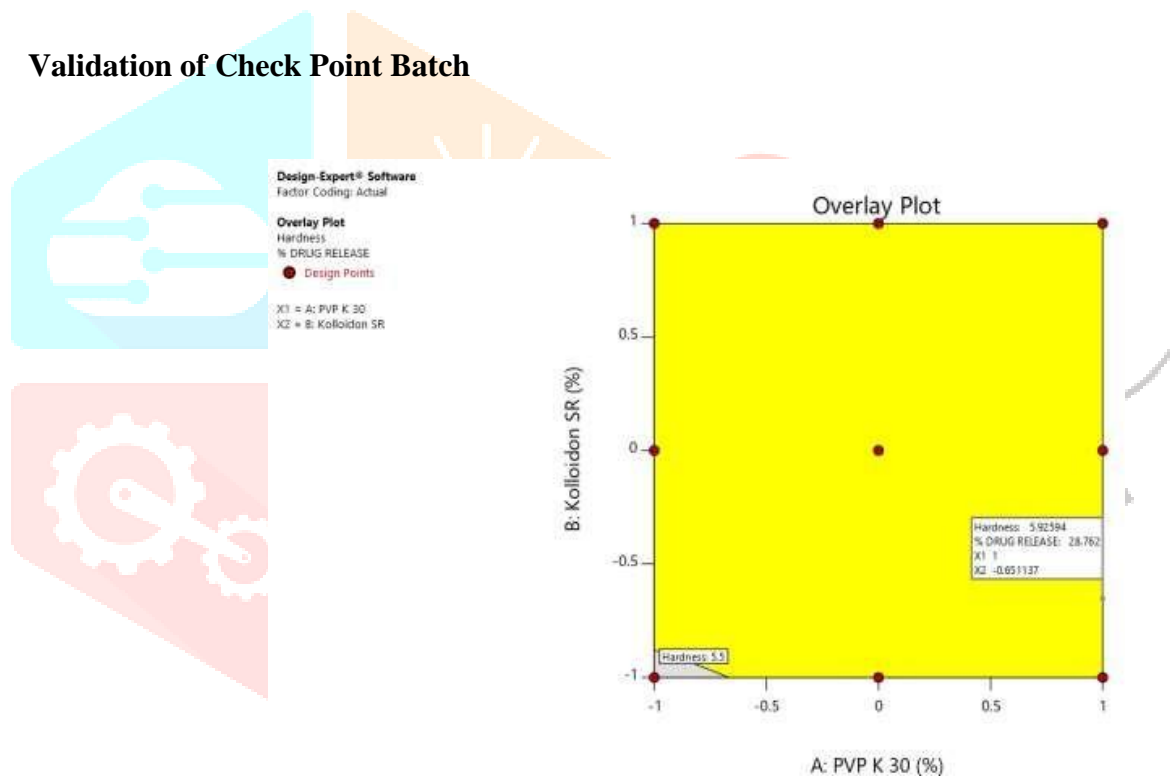


Figure 25 Check point batch figure for sustained release

Table 38 Optimized batch formulation

Ingredient	FIR8	Ingredient	FSR5
Etoricoxib	60	Etodolac	400
MCC 101	38.	MCC 101	60
Lactose	120	Lactose	47
Starch	6	PVP K 30	15
Crosspovidone	12.5	Kolloidon SR	60
Magnesium Stearate	4	Magnesium Stearte	8
Talc	6	Talc	10

Aerosil	3	-	-
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Table 39 Evaluation parameter of optimized batch

Bilayer Tablet	Hardness (kg/cm ²)	Friability (%)	Disintegration time (sec)	% drug release	Assay (%)
Etoricoxib	5.7	0.62	36 sec	98.5	96.9
Etodolac				97.2	97.5

Table 40 Drug release data of optimized batch

Time (min)	% drug release of Etoricoxib	% drug release of Etodolac
0	0	0.00
5	29.32	0.53
10	48.75	2.36
15	63.41	5.42
20	81.96	9.26
25	92.47	13.35
30	98.55	16.23
60	-	29.13
120	-	33.66
180	-	41.92
240	-	48.78
300	-	56.44
360	-	63.82
420	-	69.19
480	-	75.93
540	-	82.28
600	-	88.74
660	-	94.46
720	-	98.62

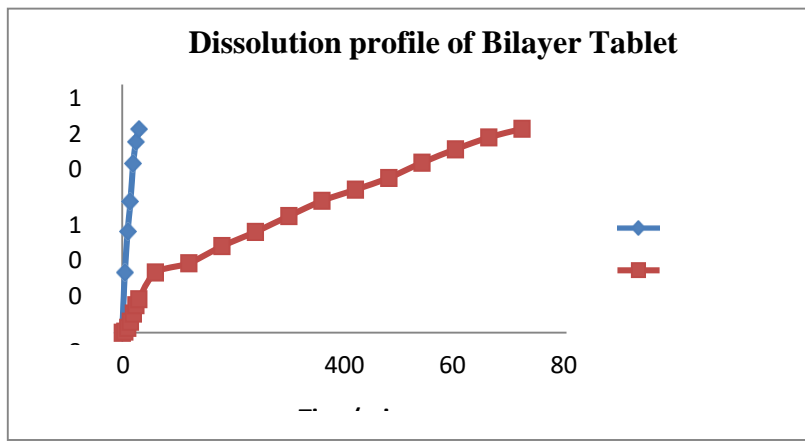
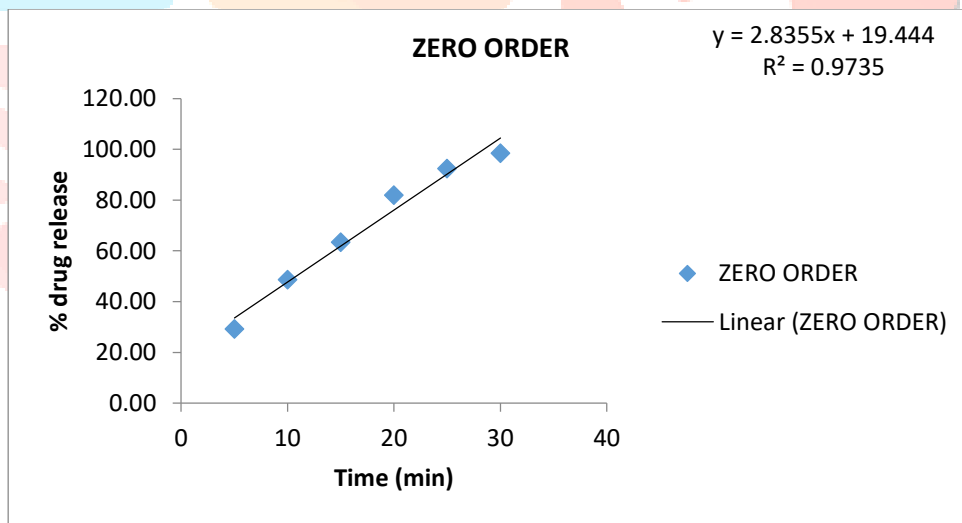


Figure 26 Drug release profile of bilayer tablet batch

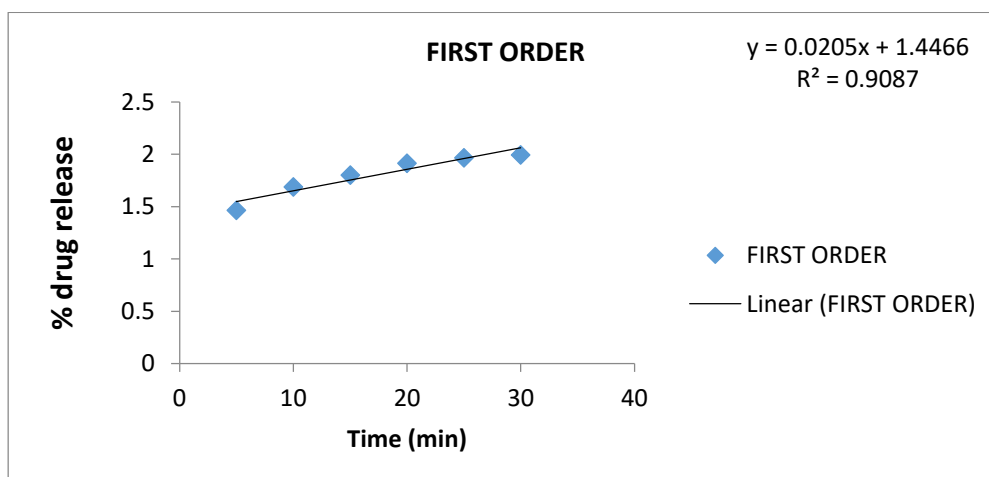
Table 41 Kinetic release data of bilayer tablet

FORMULATIONS	ZERO ORDER	FIRST ORDER	HIGUCHI MODEL	KORS PEPAS
Immediate release	0.973	0.908	0.992	0.994
Sustained release	0.997	0.978	0.996	0.997

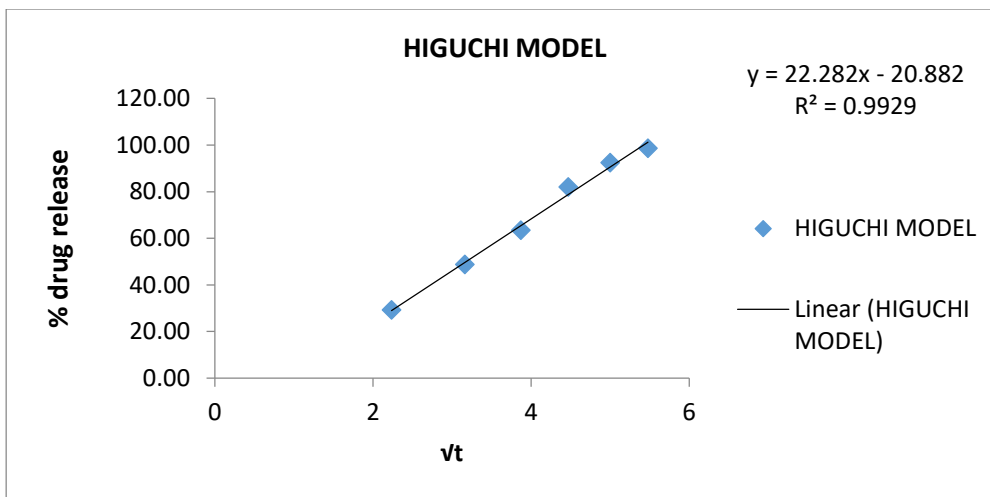
This optimized batch was selected and evaluated. The Prepared tablet were found satisfactory in physical as well as chemical evaluation. The tablet have uniform drug distribution hence drug content was found satisfactory. Diintegration time also found in acceptable limit. Drug release profile of immediate at 30 min found 98.5%. and in sustained release at 12 hours found 97.2%. Finally optimized batch was located for stability for 1 month.



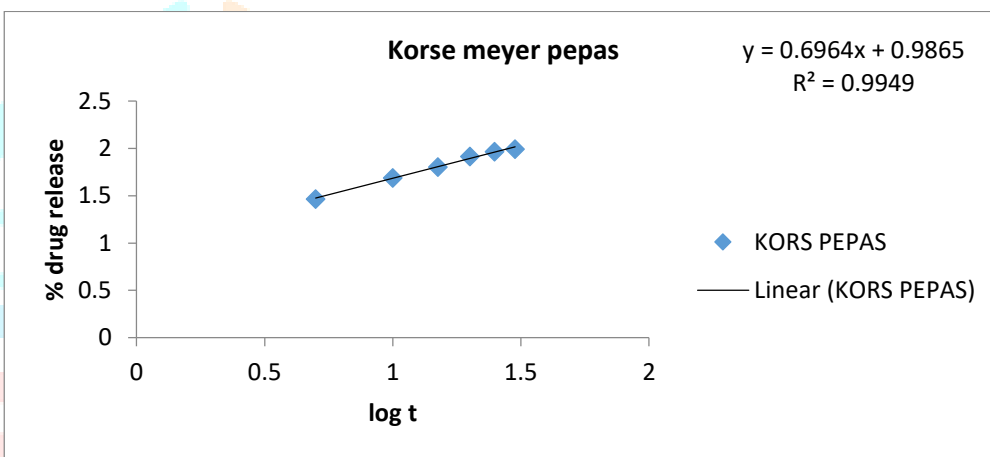
[A]



[B]

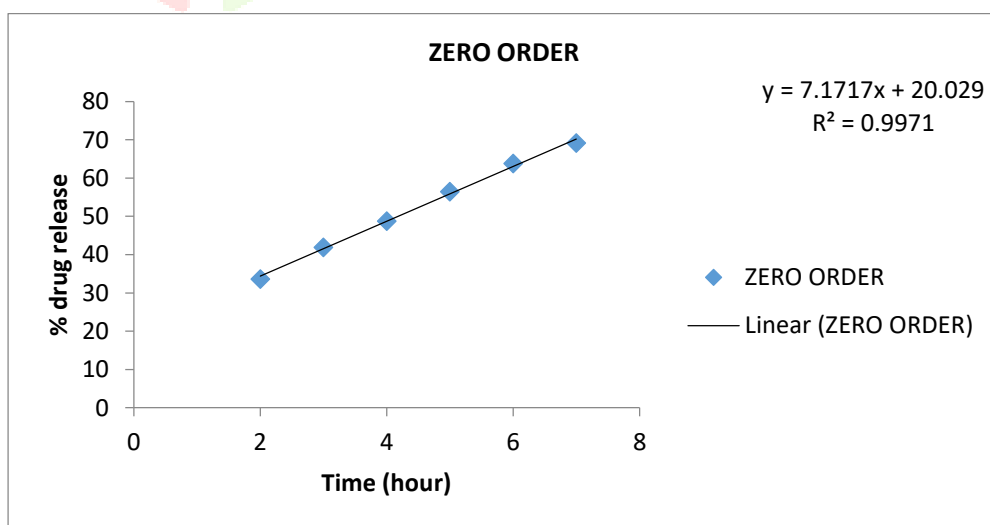


[C]

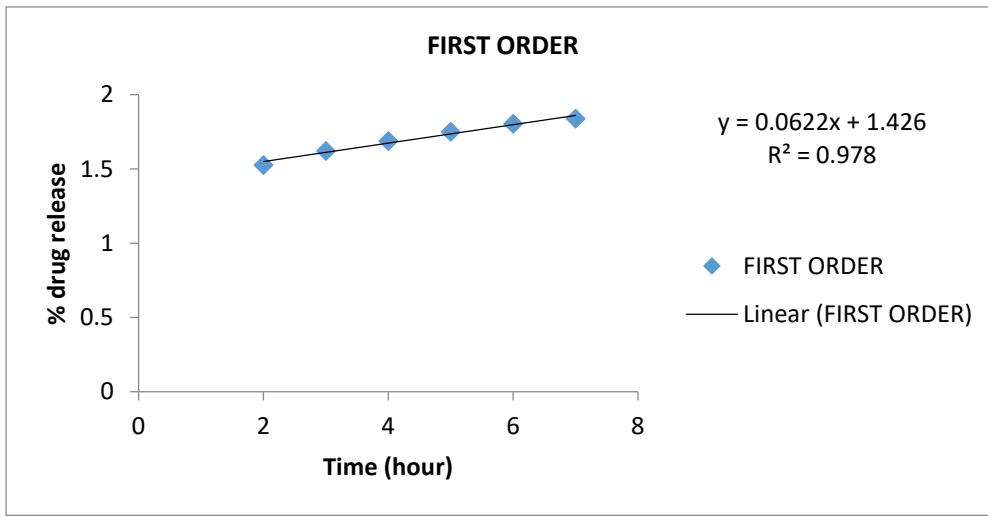


[D]

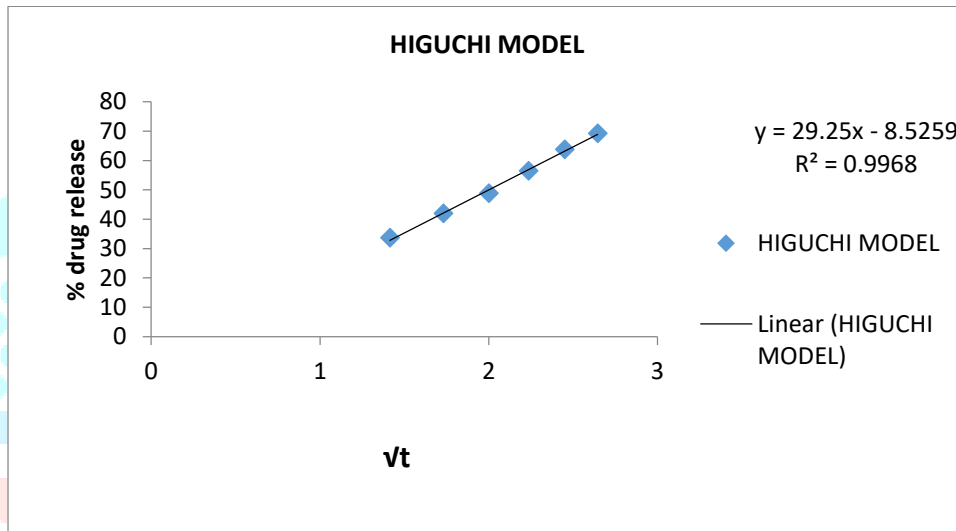
Figure 27 Kinetic release of optimized batch of immediate release [A] Zero order [B] First order [C] Higuchi model [D] Kores meyer pepas model



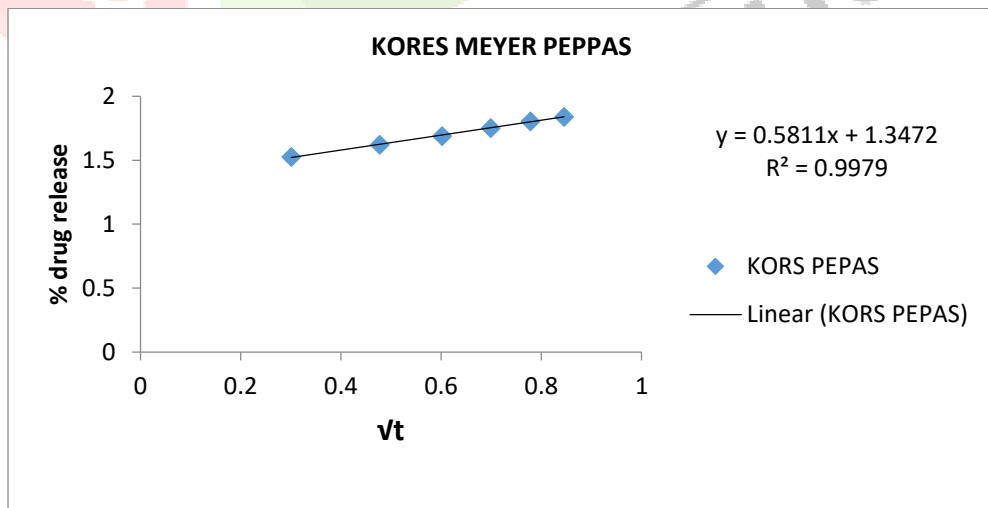
[A]



[B]



[C]



[D]

Figure 28 Kinetic release of optimized batch of sustained release [A] Zero order [B] First order [C] Higuchi model [D] Kores meyer peppas model

Stability Study

The optimized batch, O1, which exhibited superior results compared to other batches, was chosen for stability assessment. The stability study was conducted for one month under conditions of 40°C temperature and 75% relative humidity in a stability chamber. After the one-month duration, samples were withdrawn for analysis. The results indicated no alteration in the in-vitro drug release profile after 12 hours. Furthermore, the stability study demonstrated that the percentage drug content remained within the acceptable range. Additionally, there were no observable changes in the outer appearance of the tablets.

Table 42 Results of stability study of batch

Parameter		Initial	After 30 days
Appearance		White to off white tablet	White to off white tablet
Disintegration Time (sec)		36	40
Hardness (kg/cm ²)		5.7	5.6
Drug content	Etoricoxib	96.9	96.5
	Etodolac	97.6	97.5
% drug release	Etoricoxib	98.5	98.0
	Etodolac	97.2	96.9

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